

Targeted therapy using nanotechnology: focus on cancer

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Abstract: Recent advances in nanotechnology and biotechnology have contributed to the development of engineered nanoscale materials as innovative prototypes to be used for biomedical applications and optimized therapy. Due to their unique features, including a large surface area, structural properties, and a long circulation time in blood compared with small molecules, a plethora of nanomaterials has been developed, with the potential to revolutionize the diagnosis and treatment of several diseases, in particular by improving the sensitivity and recognition ability of imaging contrast agents and by selectively directing bioactive agents to biological targets. Focusing on cancer, promising nanoprototypes have been designed to overcome the lack of specificity of conventional chemotherapeutic agents, as well as for early detection of precancerous and malignant lesions. However, several obstacles, including difficulty in achieving the optimal combination of physicochemical parameters for tumor targeting, evading particle clearance mechanisms, and controlling drug release, prevent the translation of nanomedicines into therapy. In spite of this, recent efforts have been focused on developing functionalized nanoparticles for delivery of therapeutic agents to specific molecular targets overexpressed on different cancer cells. In particular, the combination of targeted and controlled-release polymer nanotechnologies has resulted in a new programmable nanotherapeutic formulation of docetaxel, namely BIND-014, which recently entered Phase II clinical testing for patients with solid tumors. BIND-014 has been developed to overcome the limitations facing delivery of nanoparticles to many neoplasms, and represents a validated example of targeted nanosystems with the optimal biophysicochemical properties needed for successful tumor eradication.

Keywords: cancer, nanomedicine, targeted nanoparticles, BIND-014

Introduction

The application of nanotechnology in medicine is providing significant opportunities and new perspectives for novel and effective treatments in many disorders, with great potential in health care. Nanomedicine can be defined as the design and development of therapeutics and/or diagnostic agents in the nanoscale range (with diameters ranging from 1 nm to 1,000 nm), with the possibility, by moving within biological systems, to transport and deliver a variety of biomedical entities for the treatment, prevention, and diagnosis of many diseases (Figure 1).¹⁻⁵

Biological transport processes, from external barriers (skin and mucosa), en route compartments (blood and extracellular matrix), and cellular membranes, to destinations at the cellular and subcellular levels are affected by the physical features of nanocarriers, including their size, shape, surface charge, and intrinsic chemical properties, as well as the incorporation of active ligands for recognition of biological receptors.⁶⁻¹⁰

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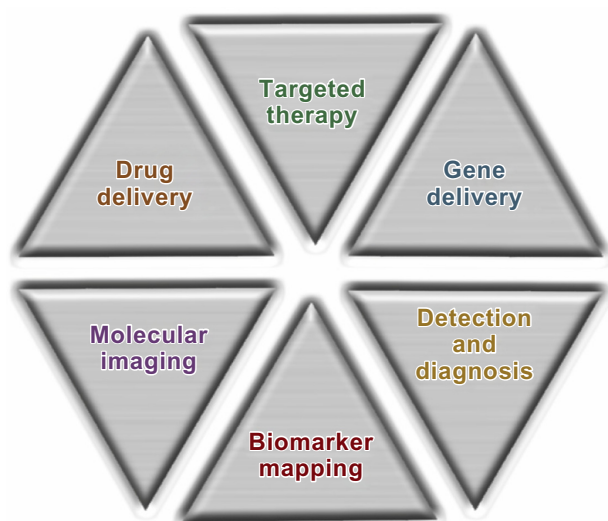


Figure 1 Biomedical applications of nanotherapeutics.

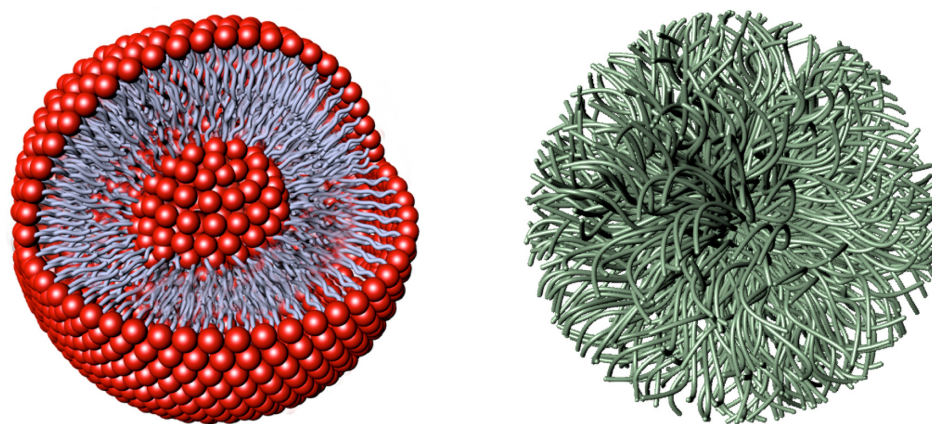
Due to their unique characteristics, including large surface area, structural properties, and long circulation time in blood compared with small molecules, nanoparticles have emerged as attractive candidates for optimized therapy through personalized medicine.^{11,12} Potential advantages of engineered therapeutic nanoparticles are the ability to: revert unfavorable physicochemical properties of bioactive molecules to desirable biopharmacologic profiles; improve delivery of therapeutics across biological barriers and compartments; control release of bioactive agents; enhance therapeutic efficacy by selective delivery of therapeutics to biological targets; and perform theranostic functions by combining multimodal imaging and simultaneous diagnosis and therapy into multifunctional nanoplatforms.^{13–18}

Over the last few decades, many original tools have been developed based on various components from metals to proteins, including carbon, silica oxides, metal oxides, nanocrystals, lipids, polymers, dendrimers, and quantum dots, as well as newly developed materials.^{1,2,4,9,19–23} For example, carbon nanomaterials with a carbon cage (eg, fullerenes, nanodiamonds) and graphene structures (eg, carbon nanotubes, nanohorns) have been explored as carriers for drug delivery and other biomedical applications,^{24–27} due to their high variability, chemical stability, and unique characteristics, such as highly tailorable surface chemistry and high carrier capacity, and the feasibility of incorporating a variety of molecules as anticancer therapeutics. However, to enable drug delivery platforms, the major emphasis should lie in investigation of the mechanism, thermodynamics, and kinetics of adsorption/desorption equilibria for putative drugs on/from carbon nanomaterials with differing purity, surface

chemistry, and agglomeration state under different conditions. Moreover, a detailed understanding of the pharmacologic and toxicologic properties of these nanomaterials, and a balanced and detailed evaluation of their risks and benefits to human health, are expected before their translation into clinical use. New perspectives using innovative nanomaterials for cancer treatment have been offered by a multifunctional platform based on gold nanoparticles, with the possibility of combining imaging and therapy, and also implementing multiple receptor targeting.^{28–32} Gold nanospheres, nanorods, nanoshells, and nanocages, for example, are currently being investigated for *in vivo* imaging, cancer therapy, and drug delivery. In particular, most studies of gold nanoparticle-based cancer therapy have involved a photothermal approach by near-infrared region laser exposure for the destruction of cancer cells or tumor tissue, which might have great potential in the clinical setting.^{29–31} Thus, laser-exposed gold nanoparticles could act as therapeutic agents by themselves without the need for co-conjugated drugs. In addition, gold nanoparticles have been used in exploratory drug delivery applications by: partitioning and diffusion-driven release of hydrophobic drug molecules; loading therapeutics by surface complexation; anchoring drugs directly to particle surfaces; loading by layer-by-layer assembly; and loading drugs inside nanoparticles.³²

As far as drug delivery is concerned, the most important nanoparticle platforms are liposomes, polymer conjugates, polymeric micelles, dendrimers, nanoshells, and protein and nucleic acid-based nanoparticles.^{1–3,6,7} Among these, the two prominent types of nanoparticles, ie, liposomes and polymer-based nanoformulations, constitute the majority of the nanoparticle therapeutics available for clinical use (Figure 2).^{7,10,15,33–40}

Although these materials are likely to provide a high degree of biocompatibility, their utilization in biomedicine requires controlled interactions with biomacromolecules. To translate developed nanomedicines into clinical practice successfully, several issues, including a favorable blood half-life and physiologic behavior with minimal off-target effects, effective clearance from the human organism, and minimal or no toxicity to healthy tissues in living organisms, should be taken into consideration.^{10,41} More specifically, hydrodynamic diameter, surface charge, and hydrophobic/hydrophilic balance are important physicochemical properties that can affect the *in vivo* biodistribution and clearance of administered nanoparticles.^{10,42} For example, optimal nanoparticle surface modification using appropriate biocompatible and biodegradable polymers, such as polyethylene glycol (PEG), constitutes a suitable strategy to reduce opsonization and uptake processes in the reticuloendothelial system, also facilitating efficient



Liposomes

Polymeric nanoparticles

Figure 2 Representative nanocarriers for drug delivery, ie, liposomes (left) and polymeric nanoparticles (right). Liposomes are self-assembling vesicles with a bilayered membrane structure containing amphiphilic molecules (phospholipids) and hydrophobic and hydrophilic groups that self-assemble in water. Polymeric nanoparticles are biocompatible and biodegradable polymeric nanoformulations in which drugs are dissolved, entrapped, or conjugated to the surface of the nanoparticles.

clearance of nanoparticles and/or their metabolites from the body.^{36,43–47} Therefore, to achieve a favorable blood half-life and biodistribution with minimal recognition and elimination by the reticuloendothelial system, great effort should be devoted to optimizing the physicochemical profile of nanoparticles.

This review highlights recent advances in the development of targeted controlled-release nanoparticles for antitumor chemotherapy, starting from the potential impact of nanotechnology in medicine, through to the clinical development of emerging passive and active targeting nanoparticles for effective controlled drug delivery. Moreover, the evolution of BIND-014, the first clinically tested targeted nanomedicine for management of cancer, as well as its pharmacobiologic properties and potential within the chemotherapeutic arena, are herein detailed.

Emerging and current nanomedicines and targeting methods: focus on cancer

The incidence of cancer has been increasing in recent decades, and eradication of the major types of the disease remains an elusive clinical goal, largely due to the heterogeneous and idiosyncratic nature of individual cancers, and the inability to target therapeutics to neoplastic areas without damaging normal tissues.^{48,49} Most of the antitumor agents currently administered by validated therapeutic protocols are systemically distributed without preferential localization to cancer tissue. This widespread biodistribution of chemotherapeutics results in both anticancer effects and off-target adverse effects. Thus far, a few nanotherapeutic (and diagnostic) materials have been approved by the US Food and Drug Administration (FDA) for clinical use, although more are currently in various stages

of preclinical and clinical development. Given that most of these products were not specifically designed to have selectivity toward biological targets, they should be considered as first-generation nanomedicines.^{1,2,7,8,9,10,40}

First generation of clinically approved nanomedicines

Among a wide variety of nanosystems, only a few nanomedicines, such as Doxil[®] (Janssen Biotech Inc., Horsham, PA, USA), Myocet[®] (Sopherion Therapeutics Inc., Princeton, NJ, USA), DaunoXome[®] (Galen US Inc., Souderton, PA, USA), Depocyt[®] (Pacira Pharmaceuticals Inc., San Diego, CA, USA), Abraxane[®] (Celgene Corporation, Inc., Berkeley Heights, NJ, USA), Genexol-PM[®] (Samyang Biopharmaceuticals Corporation, Jongno-gu, Seoul, Korea), and Oncaspar[®] (Enzon Pharmaceuticals Inc., Bridgewater, NJ, USA), are approved for use in the treatment of cancer (Table 1).

Doxil, the first nanomedicine to secure regulatory approval by the FDA (for the treatment of Kaposi's sarcoma in 1995 and in Europe in 1997 with the brand name Caelyx[®]), was obtained by encapsulating doxorubicin within liposomes.^{50,51} This nanoformulation consistently improved the pharmacokinetics and biodistribution profile of doxorubicin, thus facilitating a longer circulation half-life and maximizing drug accumulation in tumor tissue. However, despite clinical validation of this representative prototype of liposome technology in the treatment of metastatic breast cancer, ovarian cancer, and multiple myeloma, this class of nanovehicles generally fails to provide the controlled release and stability needed to control the kinetic profile and drug localization at the target tumor tissue. The non-PEGylated liposomal doxorubicin formulations, Myocet

Table 1 Examples of nontargeted nanosystems in clinical use for anticancer therapy

Name	Formulation	Bioactive compound	Indication	Status
Liposomes				
DaunoXome®	Non-PEGylated liposomes	Daunorubicin	Kaposi's sarcoma	Approved
Myocet®	Non-PEGylated liposomes	Doxorubicin	Breast cancer	Approved
Onco TCS®	Non-PEGylated liposomes	Vincristine	Non-Hodgkin's lymphoma	Approved
Depocyt®	Non-PEGylated liposomes	Cytarabine	Leukemia	Phase III
			Glioblastoma	Phase I/II
Doxil®/Caelyx®	PEGylated liposomes	Doxorubicin	Breast cancer, ovarian cancer, multiple myeloma, Kaposi's sarcoma	Approved
Thermodox®	PEGylated liposomes	Doxorubicin	Liver cancer, breast cancer	Phase III
SPI-77	PEGylated liposomes	Cisplatin	Ovarian cancer	Phase II
NL CPT	PEGylated liposomes	Irinotecan	Glioma	Phase I
Polymeric nanoparticles				
Genexol-PM®	PEG-poly(lactic acid)	Paclitaxel	Breast cancer, lung cancer, ovarian cancer	Phase II
NK105	PEG-poly(aspartic acid)	Paclitaxel	Gastric cancer	Phase I
			Breast cancer	Phase III
NK911	PEG-poly(aspartic acid)	Doxorubicin	Various solid tumors	Phase II
Opaxio™	PGA-paclitaxel	Paclitaxel	Lung cancer, ovarian cancer	Phase III
CRLX101	PEG-cyclodextrin	Camptothecin	Non-small-cell lung cancer	Phase II
NC-6004	PEG-poly(glutamic acid)	Cisplatin	Pancreatic cancer	Phase II
ProLindac™	HPMA	DACH-Pt	Ovarian cancer	Phase II
Other				
Abraxane®	Albumin-based	Paclitaxel	Breast cancer	Approved
Paclical®	Micellar retinoid-derived	Paclitaxel	Ovarian cancer	Phase III
NC-4016	Micellar PEG/polyamino acid	Oxaliplatin	Various solid tumors	Phase I/II
Oncaspar®	PEG-L-asparaginase	Asparagine specific enzyme	Acute lymphoblastic leukemia	Approved

Note: DaunoXome® (Galen US Inc., Souderton, PA, USA); Myocet® (Sopherion Therapeutics Inc., Princeton, NJ, USA); Onco TCS® (Inex Pharmaceuticals Corp., Burnaby, BC, Canada, and Enzon Pharmaceuticals Inc., Bridgewater, NJ, USA); Depocyt® (Pacira Pharmaceuticals Inc., San Diego, CA, USA); Doxil®/Caelyx® (Janssen Biotech Inc., Horsham, PA, USA / Janssen-Cilag Pty Ltd, Macquarie Park, NSW, Australia); Thermodox® (Celsion Corporation, Lawrenceville, NJ, USA); Genexol-PM® (Samyang Biopharmaceuticals Corporation, Jongno-gu, Seoul, Korea); Opaxio™ (Cell Therapeutics, Inc., Seattle, WA, USA); ProLindac™ (Access Pharmaceuticals Inc., Dallas, TX, USA); Abraxane® (Celgene Corporation, Inc., Berkeley Heights, NJ, USA); Paclical® (Oasmia Pharmaceutical AB, Uppsala, Sweden); Oncaspar® (Enzon Pharmaceuticals Inc., Bridgewater, NJ, USA).

Abbreviations: PEG, poly(ethylene glycol); HPMA, hydroxypropylmethacrylamide; DACH-Pt, diamincyclohexane-platinum.

and DaunoXome, have been used for metastatic breast cancer and Kaposi sarcoma, respectively.^{52,53} Further, DepoCyt, a non-PEGylated liposomal nanocarrier loaded with cytarabine, was approved in 1999 for local intrathecal treatment of lymphomatous meningitis, and has now entered Phase III trials for leukemia and Phase I/II clinical trials for glioblastoma.⁵²

Another therapeutic nanoformulation to secure clinical approval by the FDA (in 2005) is Abraxane, a co-condensate of albumin and paclitaxel.⁵³ In comparison with paclitaxel formulated using Cremophor® EL (the nonionic surfactant used in the Taxol® formulation), Abraxane demonstrated significantly higher tumor response rates and longer times to tumor progression in patients with metastatic breast cancer. However, the utility of this technology is mainly limited to improving the therapeutic index of hydrophobic therapeutic agents (able to bind to albumin) used in formulations with poorly tolerated vehicles.

More recently, in 2007 in Korea, another polymeric nanocarrier was approved for marketing, ie, Genexol-PM,

a paclitaxel-loaded poly(lactic acid)-block-poly(ethylene glycol) micelle formulation, that was developed to avoid the need to use Cremophor EL.⁵⁴ Genexol-PM led to an increase in the potency of paclitaxel in the treatment of breast and lung cancer, and is currently in Phase II clinical development in the US and Russia. With regard to PEGylated devices, Oncaspar, a combination of PEG-L-asparaginase, has recently been approved for the treatment of leukemia.⁵²

Liposomes and polymeric drug release nanoformulations in clinical development

Despite the progress made in the clinical development of liposome-based nanocarriers, there are several issues that limit their wider consideration as a main drug delivery platform, including the difficulty in modulating their drug release in vivo, the limited amount of drug that can be loaded, possible oxidation of liposomal phospholipids, and the difficulty in

maintaining a stable shelf-life. Otherwise, polymeric nanocarriers demonstrate similar to superior stability *in vivo* as compared to liposomes, have a high drug-loading capacity, and enable both controlled and triggered release of drugs. Therefore, polymeric-based nanomaterials have the potential to provide solutions for a range of problems in nanomedicine.^{40,55–58}

The way forward for the clinical translation of controlled-release polymeric nanoparticles was paved by the seminal work of Langer and Folkman in 1976, which demonstrated the controlled release of macromolecules from biodegradable polymers in a temporal manner.³⁶ Moreover, a landmark paper by Langer et al in 1994 provided further evidence that diblock copolymers of biocompatible polymers with PEG can dramatically increase the controlled release and circulation half-life of polymeric nanoparticles.³⁷ Because of their biocompatibility, biodegradability, and chemical and technologic flexibility, the polymeric materials most widely used for controlled drug release include PLA, poly(D,L-lactide-co-glycolide) (PLGA), poly(caprolactone) (PCL),

poly(glutamic acid), N-(2-hydroxypropyl)-methacrylate copolymers, and poly(amino acids).⁵⁶

“Drug-targeting” strategies

Since Paul Ehrlich, considered the “father of chemotherapy”, suggested the concept of a “magic bullet”, ie, “a drug that selectively attaches to diseased cells but is not toxic to healthy cells” approximately a century ago,⁵⁹ a great deal of interest has been channeled in this direction, focused particularly on the treatment of cancer.⁶⁰ Several strategies can be exploited to reach a putative biological target, and include passive drug targeting, active drug targeting, active drug targeting to endothelial cells, and triggered drug delivery (Figure 3Aa–Dd).^{6–8,10,12,40,56–58}

Passive drug targeting

The majority of nanosystems show prolonged blood circulation times *in vivo* and accumulate at particular sites simply due to the balance between vascular hemodynamic forces

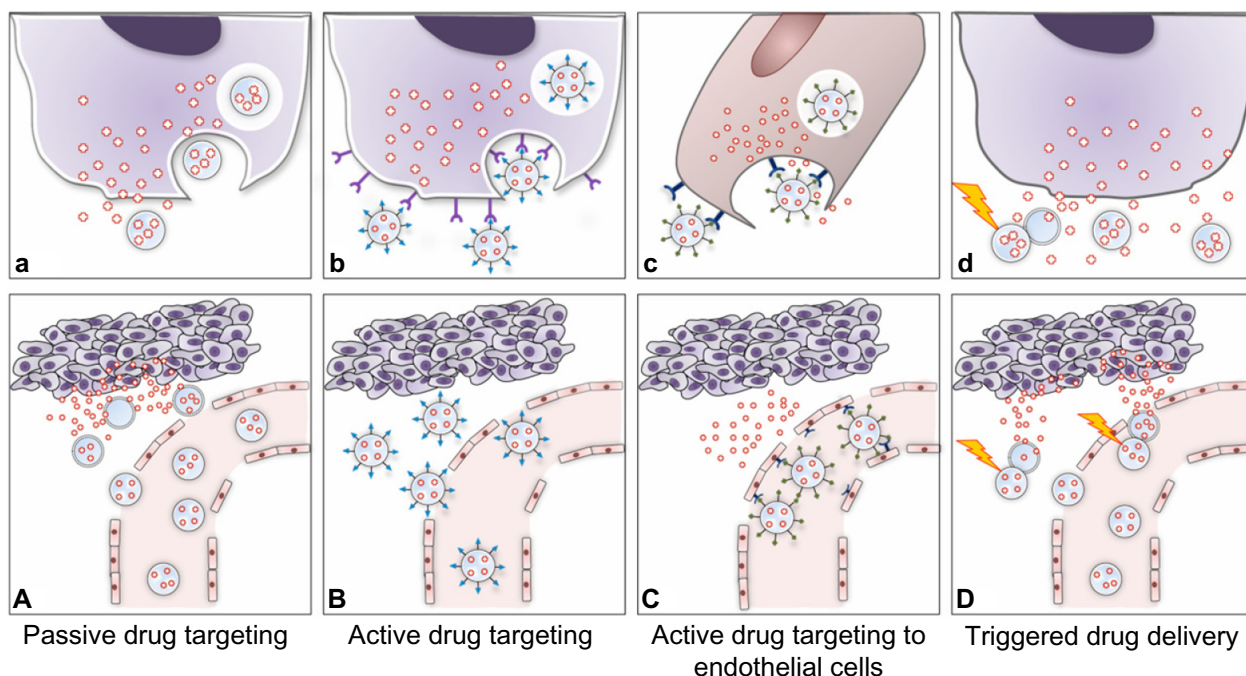


Figure 3 Strategies adopted for drug targeting and localization of nanosystems to tumor cells and tissues.

Notes: (A) Passive drug targeting. Circulating nanoparticles passively extravasate in solid tumor tissue via the enhanced permeability of blood vessels, ie, through the disorganized and leaky vasculature surrounding the solid tumor coupled with the absence of lymphatic drainage, and preferentially accumulate in tumor cells (the EPR effect). (a) The drug is released into the extracellular matrix and diffuses through the cells and tissue. (B) Active drug delivery. Once nanoparticles passively extravasate and concentrate in the target tissue via the EPR effect, the presence of ligands grafted onto the nanoparticle surface enable active targeting of the nanoparticles to receptors that are overexpressed on tumor cells or tissue, resulting in enhanced uptake and internalization via receptor-mediated endocytosis. (b) Tumor-specific ligands on the nanoparticles bind to cell surface receptors, triggering internalization of the nanoparticles into the cell through endosomes on which, due to an internal acidic pH, the drug is released from the nanoparticles and diffuses into the cytoplasm. (C) Active drug targeting to endothelial cells. Nanoparticles can be targeted to bind to angiogenic endothelial cell surface receptors with the aims of: enhancing drug accumulation in the tumor endothelium, thereby inhibiting growth of blood vessels supplying the tumor rather than inhibiting tumor cells per se (c); and improving delivery of chemotherapeutic agents to tumor cells via the EPR effect with the potential to act synergistically in targeting both the vascular tissue and tumor cells. (D) Triggered drug delivery by stimuli-sensitive nanomedicines. Nanoparticles passively accumulate in the tumor via the EPR effect. After localization at the target site or while circulating in the tumor vasculature (d), the nanoparticles can be activated by external stimuli (eg, hyperthermia, light, magnetic fields, ultrasound) that induce release of the payload drugs. Images adapted from *J Control Release*, 161(2), Lammers T, Kiessling F, Hennink WE, Storm G, Drug targeting to tumors: principles, pitfalls and (pre-) clinical progress, 175–187, Copyright 2012, with permission from Elsevier.¹⁰

Abbreviation: EPR, enhanced permeability and retention.

and diffusion mechanisms. Passive drug targeting is widely exploited in chemotherapy because nanoparticles circulating in the bloodstream can be localized to neoplastic tissues through the well known enhanced permeation and retention effect.^{61,62} Anatomically, tumor microvasculature is leaky and characterized by abnormal branching and enlarged interendothelial gaps, with associated breakdown of tight junctions between endothelial cells and a disrupted basement membrane.⁶³ These large gaps between endothelial cells facilitate the extravasation of particulate material from the surrounding vessels into the tumor (Figure 3A).⁶⁴ Therefore, in contrast with the vasculature in healthy tissues, the poorly differentiated vasculature of immature tumors, with pores smaller than about 400 nm, allows for extravasation and selective accumulation of nanoparticles in the tumor interstitium via a passive targeting mechanism (Figure 3A).^{42,65} Importantly, it should be borne in mind that the enhanced permeation and retention effect is a very heterogeneous phenomenon, varying dramatically from tumor to tumor and from patient to patient.⁶⁶ For example, even considering a single tumor model, there are many differences with regard to vascular permeability, where particles with a diameter >200–300 nm are able to extravasate, whereas in another part of the same tumor, molecules only a few nanometers in size may have difficulty entering the interstitium.

Most passive targeting nanosystems have a surface coated with PEG for biocompatibility and “stealth” purposes.^{42–44} Importantly, it should be noted that increased hydrophilicity on the nanoparticle surface can impede its uptake by cancer cells, thereby hampering efficient drug delivery to tumors by passive targeting nanoparticles.^{42,47,67} However, PEG-based block copolymers have resulted in the clinical translation of numerous passive targeting polymeric nanoparticles, including the abovementioned Genexol-PM, as well as SP1049C, NK911, and other prototypes now entering early clinical trials for the treatment of a variety of cancers (Table 1).

SP1049C is a Pluronic polymeric micelle nanoparticle carrying doxorubicin, and is currently undergoing Phase II trials in metastatic cancer of the esophagus refractory to standard chemotherapeutic protocols.⁶⁸ Another example of a polymeric nanocarrier that acts via a passive targeting mechanism is NK911, a micellar nanoparticle comprising PEG, doxorubicin, and poly(aspartic acid), currently in Phase II clinical development for various types of cancer.⁶⁹ Moreover, Opaxio™ (formerly Xyotax™), also a passively targeted paclitaxel/poly(L-glutamic acid) nanoconstruct, is proving effective in ovarian tumors,^{70,71} and CRLX101 (formerly IT-101), a camptothecin-cyclodextrin polymer

conjugate, is showing enhanced pharmacokinetic efficacy in both preclinical and clinical studies.⁷² Further conjugated polymer-drug nanotherapeutics, such as NC-6004 [a cisplatin-incorporated PEG-poly(glutamic acid) block copolymer micellar formulation] and ProLindac™ (a diaminocyclohexane-platinum hydroxypropylmethacrylamide prodrug), are in late-stage clinical trials.¹⁰ In addition, Paclical®, a micellar formulation of paclitaxel, has recently received orphan drug designation by the FDA, and is currently in Phase III trials for ovarian carcinoma.⁷³ Passive targeting lipid nanocarriers are also moving into the advanced stages of clinical trials, and intensive effort is being made to get these systems into clinical practice (Table 1). Promising liposomal nanomedicines in clinical trials include Thermodox®, a thermosensitive liposomal doxorubicin formulation that releases the active drug at temperatures around 39°C, and is currently being tested in Phase III trials together with radiofrequency ablation in patients with hepatocellular carcinoma.⁷⁴ Finally, SPI-77, a PEGylated liposomal formulation of cisplatin, is in Phase II trials for patients with recurrent epithelial ovarian cancer,⁷⁵ and a nanoliposomal formulation of irinotecan (CPT-11) is in Phase I trials for glioma.⁷⁶ Several liposomal formulations carrying two different types of chemotherapeutics, such as cytarabine and daunorubicin, are also reported to be in the process of clinical development.⁷⁷

Active targeting as a strategy for developing site-directed nanoparticles

Passive targeting strategies have shown several limitations, so a considerable amount of work is now underway investigating active targeting nanoformulations that can maximize their accumulation at sites of interest.^{7,8,10} In this respect, polymeric nanoparticles allow for versatile modification possibilities, and can act as functional platforms for the assembly of well defined multifunctional structures.^{40,56–58,78} In fact, slight variations in polymeric composition as well as ligand surface functionalization can facilitate the targeting ability of nanoparticles in biological systems. Active drug targeting involves the use of a variety of affinity ligands to direct the binding of nanoparticles to many biological targets, largely represented by antigens, that are differentially overexpressed both in the plasma membrane and in diseased tissue (Figure 3B and b).^{40,79} This approach can be used for controlled drug release applications, where the drug is released into either the extracellular or intracellular compartment. In the latter process, internalization of nanoparticles by receptor-mediated endocytosis can occur through several pathways that lead to endosome formation, and ultimately

allow for generation of lysosomes (Figure 3b).^{56,80} Since the primary role of the targeting ligand is to enhance the uptake of nanoparticles into target cells, cell internalization by active targeting nanoparticles is postulated to improve the therapeutic efficacy as compared with nontargeted nanoparticles.^{56–58} This suggests that while the biodistribution would be strictly related to the colloidal properties of the nanoparticles, the targeting ligand is important for enhancing both cell recognition and cell uptake at target sites. While the potential benefit of active targeting nanoparticles seems to be widely accepted, this technology has resulted in only a few clinically validated nanoproducts (Table 2).^{10,40,58}

Active drug targeting to endothelial cells and triggered drug delivery

Several important pitfalls in active targeting of drugs to tumor cells have been identified, including: poor tumor penetration by nanomedicines; the complexity of predicting the potential usefulness of an active drug targeting approach for a specific application; difficulty in managing nanoformulations that are too complex in design; the not always favorable implementation of nanomedicine formulations in clinically consistent combination regimens; and the low level of knowledge concerning the biological and (patho)physiologic principles of tumor progression and related treatment.¹⁰ Although this approach has potential in controlled and targeted drug delivery, the failure of translation of a great number of targeted nanomedicines at the clinical level can likely be attributed to the inability of targeted nanoparticles to overcome a succession

of membrane layers as biological barriers, represented by pericyte-based, smooth muscle cell-based, and fibroblast-based cell layers between endothelial and cancer cells, as well as a plethora of cellular processes and anatomic tumor issues (ie, the high cellular density within solid tumors and high interstitial fluid pressure) that represent important obstacles for reaching the target tumor interstitium.^{4,6,8–10,56}

To address these issues, a variety of vascular-targeted nanoformulations have been designed and evaluated (Figure 3C and c).^{8–10,56} Example of ligands targeting angiogenic endothelium are the linear and cyclic derivatives of an oligopeptide containing the Arg-Gly-Asp (RGD) sequence, that binds to target endothelium via integrin receptors.^{81,82}

Another targeting strategy capable of generating innovative nanoformulations focuses on the possibility that a nanosystem can be triggered to release its contents (ie, the payload drug) on exposure to external and confined stimuli, such as light, heat, ultrasound, and magnetic fields, in order to maximize drug release at the pathologic site (Figure 3D and 3d).¹⁰ The above mentioned product, Thermodox, a temperature-sensitive doxorubicin-PEGylated liposome, is an interesting example of stimuli-responsive nanomedicine.⁷⁴ Despite the clinical potential of these nanoformulations, there are still several important limitations to their extensive clinical development, that include manufacturing difficulties and problems with managing the way in which they respond to stimuli-responsive drug release. However, much effort has been made to improve the stimuli-responsiveness of these tumor-targeted nanotherapeutics, and the development of

Table 2 Tumor-targeted nanomedicines in clinical development

Name	Formulation	Targeting ligand	Bioactive compound	Indication	Status
Liposomes					
CALAA-01	Cyclodextrin-based NP containing anti-RRM2	Transferrin	siRNA	Various solid tumors	Phase I
MBP-426	Liposomes	Transferrin	Oxaliplatin	Gastroesophageal adenocarcinoma	Phase II
MCC-465	PEGylated liposomes	F(ab') ₂ fragment of human Ab GAH	Doxorubicin	Metastatic stomach cancer	Phase I
SGT53	Liposomes	Anti-transferrin receptor single-chain Ab fragment (TfRscFv)	p53 gene	Solid tumors	Phase I
C225-ILS-DOX	PEGylated liposomes	Antigen-binding fragments (Fab) of cetuximab	Doxorubicin	Advanced solid tumors	Phase I
Polymeric nanoparticles					
BIND-014 (Accurins™)	PEGylated PL(G)A	Small molecule	Docetaxel	Solid tumors	Phase II
Atu027	Liposomes	Protein kinase N3	siRNA	Solid tumors	Phase I
C-VISA-BikDD	Liposomes	Proapoptotic gene	BikDD plasmid DNA	Pancreatic cancer	Phase I

Note: Accurins™ (BIND Therapeutics, Inc., Cambridge, MA, USA).

Abbreviations: NP, nanoparticles; PEG, poly(ethylene glycol).

more effective nanoparticles for triggered drug delivery is expected in the near future.^{83,84}

Methods and ligands used for targeted drug delivery

In the course of the last decade, several strategies involving conjugation of targeting ligands to the surface of nanoparticles have been developed.^{38,40,45,55–57} As far as the targeting approach is concerned, one key issue relies on the choice of optimal targeting ligands, possibly by balancing their stoichiometry in comparison with the antibiofouling surface of nanoparticles. More specifically, two important ligand properties, ie, affinity and density, can have a key role in effective targeting of nanoparticles to the cell surface membrane. Again, the ligand binding affinity is the result of the equilibrium between enthalpic advantages (for ligand-receptor interaction) and entropic losses (stretching, flexibility, or compressibility of the nanosystem). For example, greater ligand density does not necessarily lead to a higher intracellular concentration, given the decrease in “stealth” surface characteristics. Moreover, although the uptake of nanoparticles usually increases with an increasing \pm charge ratio of nanoparticles (in terms of zeta potential values), an excess positive charge can induce toxicity and promote an immunologic reaction. Therefore, the optimal ligand density and charge on the nanoparticle surface should be investigated on a case-by-case basis. However, a wide range of chemical modifications is now available to attach targeting ligands to nanoparticles.^{55–57,85}

Conventional methods of preparing targeted nanoparticles involve two typical options, ie, the “postcoupling” and “precoupling” approaches.^{55–57} The first approach involves bioconjugation of the preformed nanoparticle core with targeting ligands to the nanoparticle surface. This postcoupling approach for attaching affinity ligands does not allow for fine-tuning of the ligand-nanoparticle surface density for optimal efficacy. Conversely, most effective chemical strategies include pre-conjugation of a targeting ligand after nanoparticle formation followed by nanoformulation (ie, the precoupling method). For example, effective self-assembly of prefunctionalized triblock polymers (ie, copolymer-PEG ligands), accomplished in the pioneering work of Farokhzad and Langer,^{86,87} demonstrated the possibility of developing more homogeneously targeted nanoparticles capable of controlling ligand-to-nanoparticle ratios and preventing a heterogenous distribution of ligands on the surface of nanoparticles. Summarizing this information, it is clear that a combination of several “unpredictable” factors, including

the nature of the targeting ligand, the size, shape, and composition of the targeted nanosystem, as well as the balance of the ligand-nanoparticle surface ratio, can synergistically contribute to the efficiency of binding between targeted nanoparticles and their target cells, and directly affect the biological profile in vivo. Therefore, all these aspects should be investigated in a rational fashion when developing a nanosystem.

Using different approaches, nanoparticles can be functionalized using a variety of targeting ligands that include monoclonal antibodies or their fragments, proteins, or peptides, nucleic acid ligands (such as aptamers), and small molecules, the characteristics of which are outlined in the following sections and summarized in Figure 4.⁸⁸

Monoclonal antibodies

Monoclonal antibodies have for several years been the preferred class of targeting ligands, and engineered monoclonal antibodies, preferably one capable of evading the immune system, have been widely used in the development of targeted nanoparticles. Current development of monoclonal antibodies has led to chimeric and humanized derivatives to enable modulation of their immunogenicity. The ability of engineered monoclonal antibodies to target and interfere with cellular processes has been demonstrated by the success of several monoclonal antibody therapeutics.^{89,90} Some of these, including rituximab and trastuzumab, have been conjugated to PLA nanoparticles, resulting in nanoconjugates that show a significant increase in the rate of particle uptake compared with their nontargeted counterparts.⁹¹ However, despite the intense effort undertaken for their development, monoclonal

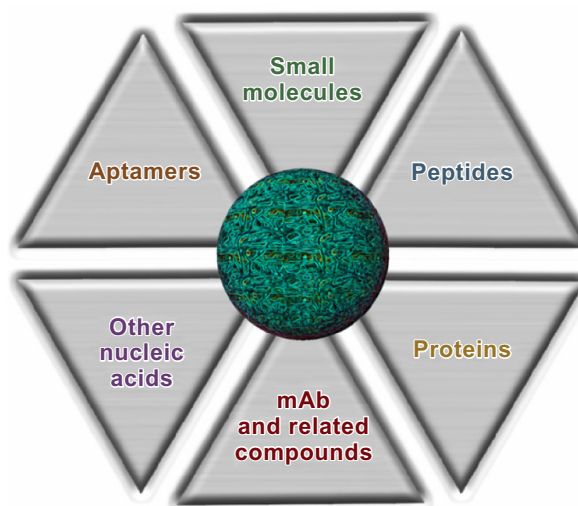


Figure 4 Types of ligands used for targeted nanoparticles. **Abbreviation:** mAb, monoclonal antibody.

antibodies still have a number of limitations, including their large size, requirement for extensive optimization through molecular engineering technologies, difficulty in managing nanoparticle scale-up and manufacturing, and potentially immunogenic characteristics, resulting in rapid nanoparticle clearance. Due to these problems in using monoclonal antibodies, there is increasing interest in engineering and using antibody fragments as targeting molecules to retain the high antigen binding specificity of the parent antibodies, but with less immunogenicity and a smaller size, and thus obtain monoclonal antibodies that are better suited for molecular targeting. These include the Fab fragments, single chain variable fragments (scFv), minibodies, diabodies and nanobodies.^{2,92}

Aptamers

Aptamers are small, single-stranded RNA or DNA sequences of oligonucleotides that can be designed as ligands capable of binding to targets with high sensitivity and specificity.^{93,94} They are small in size (usually approximately 15 kDa), and have less immunogenicity with respect to monoclonal antibodies or other macromolecules, leading to better stability and biodistribution.^{95,96} Such biomolecules fold by intramolecular interactions into unique three-dimensional conformations and topologies, having the ligand-binding characteristics needed for efficient target (receptor/antigen) affinity. Selective aptamers, with binding affinity toward a specific target, are currently being identified by an *in vitro* chemical process known as “systemic evolution of ligands by exponential enrichment” (SELEX).⁹⁷ In this process, which can be easily scaled up at a relatively low cost, a library of ten random oligonucleotides is enriched in order to identify the prototype with the highest affinity and specificity. Using this technology, Langer and Farokhzad designed and developed customized controlled-release nanoparticles loaded with docetaxel and having tumor-targeting capability toward prostate-specific membrane antigen (PSMA).^{40,86,87,98,99} Targeted nanoparticles have been obtained by decorating their shell surface with RNA A10-aptamer to bind PSMA,^{100–102} a clinically validated tumor marker that is not only overexpressed on the surface of prostate cancers but also on the neovasculature of many solid tumors. This approach constituted the proof-of principle for development of the first targeted polymeric nanoformulation (ie, BIND-014), which is now approved for clinical use (see below).

Proteins and peptide-based targeting molecules

Several endogenous proteins capable of selectively binding to specific receptors on membrane cells can be used for targeting

purposes via receptor-mediated endocytosis.¹⁰³ For example, transferrin, an iron-transporting protein that binds specifically to transferrin receptors (TfR) located on the cell surface, has been used to transport nanoparticles into different types of cells.^{103,104} However, their effectiveness for targeting purposes may be limited by their immunogenicity and susceptibility to early clearance. The target receptors for these proteins are also commonly expressed on various types of nontargeted cells, which can lead to unwanted off-target effects.

Peptide-based ligands are emerging as attractive alternative targeting molecules due to their small size, high stability, and relatively low immunogenicity as compared with many proteins. Identification of specific targeting ligands has usually derived from previously or newly focused peptide phage/bacterial/plasmid peptide display libraries, as well as use of newer and easier screening technologies.¹⁰⁵ Like monoclonal antibodies and aptamers, peptides can bind to several molecular targets with a high degree of affinity and specificity, and are easy to manufacture by conjugation to polymers, lipids, and various nanoparticle surfaces.^{106,107}

Small molecules

Small molecules, usually defined as low molecular weight organic molecules with a molecular weight <500 Da, constitute a promising class of targeting molecules because of their small size, high stability, chemical management, and low production cost.^{57,58,108} Some further advantages of small molecules as targeting ligands include: availability of suitable facile coupling chemical methods for their conjugation; the possibility to modulate ligand densities and charge on nanoparticle surfaces, since these parameters can affect stability, size, and morphology, as well as targeting efficiency; availability of a wide range of targeting ligands with variable physicochemical properties and a variety of functional groups; fewer immunogenic effects *in vivo*; and reproducible, scalable, and economical manufacturing. Among the large number of small molecules identified as potential targeting ligands, folic acid has been one of the most extensively studied and used ligands in targeted drug delivery.^{108,109} Due to its high affinity for folate receptors, which are overexpressed in many types of tumor cells, the vitamin folate has also been used to deliver drug conjugates and many drug delivery systems (ie, liposomes, polymeric nanoparticles, dendrimers) to selectively accumulate drugs into cancer cells using folate receptor-mediated endocytosis.¹¹⁰

Pomper et al have previously identified small hydrophilic molecules from a series of urea-based PSMA inhibitors as novel diagnostic agents capable of targeting the PSMA

receptor in prostate cancer cells with affinity and specificity similar to that of antibodies and aptamers.^{111–113} Interestingly, a small molecule belonging to this class of molecules, ie, the pseudomimetic dipeptide 2-[[5-amino-1-carboxypentyl] carbamoyl]amino}pentanedioic acid,¹¹¹ already used by Sechi et al for development of (–)-epigallocatechin 3-gallate-loaded PSMA-targeted nanoparticles¹¹⁴ and by Chandran et al for preparation of docetaxel-PLA/PCL-based targeted nanoparticles,¹¹⁵ was also used as a targeting ligand in the development of BIND-014.¹¹⁶

Concerning other small molecules that could be used as targeting ligands, carbohydrates, ie, sugar-based compounds, have also gained attention due to their low molecular weight, high availability and biocompatibility, and ease of production. Several of these carbohydrate ligands target membrane carbohydrate-binding proteins (membrane lectins) that are differentially expressed on the cellular and intracellular membranes, and some carbohydrates, such as mannose, glucose, galactose, and their derivatives, have been considered as potential ligands for carriers in cell-selective drug delivery.^{117,118}

The clinical translation of the above-described technologies has ushered in a new era in the development of innovative therapeutic nanoparticles that are capable of targeting and controlled release, also considering the possibility of codelivery of multiple active agents.

Clinical development of targeted nanoparticles

To date, only three targeted liposomes and four targeted polymeric nanoparticles have progressed in clinical development (Table 2). The prototype that reach clinical trials was MCC-465, a new generation of liposome-encapsulated doxorubicin with a surface covered by both PEG and antigen-binding fragments [F(ab')₂] to confer immune shielding and targeting, respectively, that is used in the treatment of human stomach cancer.¹¹⁹ Another site-directed liposome is SGT53-01, a TfR-functionalized nanoformulation containing a chain antibody fragment (TfRscFv) as the targeting ligand. It has been designed to carry the p53 tumor suppressor gene to cancer cells, and is currently undergoing Phase I clinical trials in combination with doxorubicin for the treatment of solid tumors.¹²⁰ The third site-specific liposomal nanocarrier is MBP-426, a TfR-targeted liposome encapsulating oxaliplatin, that has been used clinically for the treatment of a variety of solid tumors.^{121,122}

With regard to targeted polymeric nanoformulations, CALAA-01 was the first nanotherapeutic to reach clinical

development for siRNA delivery in 2008.¹²³ This nanosystem consists of TfR-targeted cyclodextrin-based PEGylated nanoparticles containing siRNA, and is capable of reducing expression of the M2 subunit of ribonucleotide reductase. The safety of CALAA-01 was evaluated in a Phase I clinical trial by intravenous administration to adults with solid tumors refractory to standard of care therapies.¹²⁴

More recently, a new antiepidermal growth factor receptor nanoimmunoliposome loaded with doxorubicin (ie, C225-ILS-DOX) entered Phase I investigation for the treatment of solid tumors.¹²⁵ Fab fragments of the chimeric monoclonal antibody cetuximab (C225, Erbitux) were covalently conjugated to the liposome membrane to target nanoparticles against tumor cells overexpressing EGFR (Table 2).¹²⁶

Focusing on the first clinically tested targeted nanomedicine, a major effort has made on BIND-014 (Table 2),¹¹⁶ a new docetaxel formulation developed by a team led by Langer and Farokhzad at the Massachusetts Institute of Technology, Harvard Medical School, and BIND Therapeutics, as a programmable nanomedicine that recently entered Phase II clinical testing for the treatment of patients with solid tumors (Figure 5). The development of BIND-014, along with its pharmacobiologic profile and potential clinical outcomes, is discussed in the following sections.

Pharmacology, mode of action, and pharmacokinetics of BIND-014

Development of BIND-014

The clinical translation of a targeted drug delivery nanosystem is strictly related to an optimal and synergistic combination of several physicochemical features, including polymer type, size, surface charge, hydrophilic/hydrophobic balance, ligand type and density, drug properties (type, solubility, loading, kinetics), and in vivo release capability (ie, tissue penetration, navigation across membrane layers and biological barriers, immune evasion or “stealth” characteristics, and cellular binding, uptake, and internalization processes).^{8,40,56,58,116}

Considering these issues, BIND Biosciences (now BIND Therapeutics) developed customized controlled-release nanoparticles by using new high-throughput technology to achieve multifactorial optimization of polymeric nanosystems. The history of this project started with the pioneering work of Langer and Farokhzad that led to proof-of-concept for the development of innovative drug delivery vehicles composed of several safe or FDA-approved materials as biocompatible polymers (ie, PLA, PLGA, and PEG) and aptamers to target PSMA.^{40,85,86} Such nanoparticles were loaded with docetaxel, a semisynthetic taxane and one of the most commonly

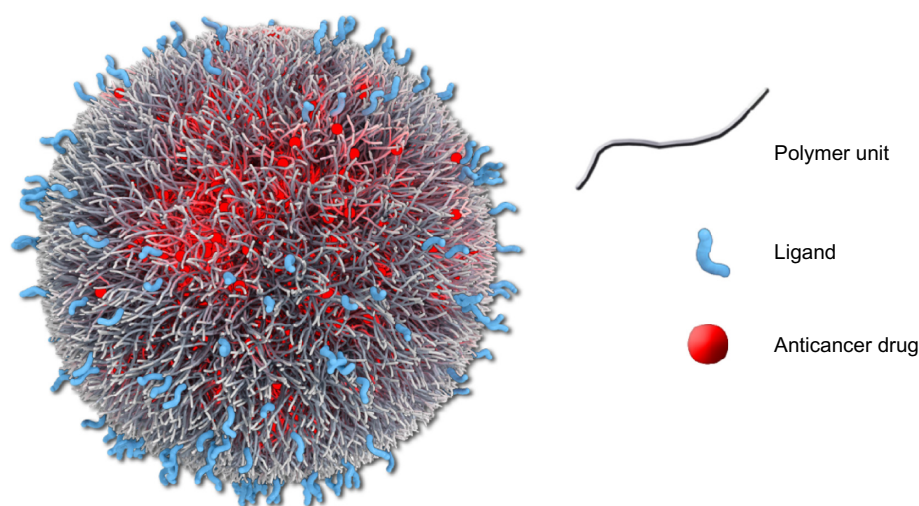


Figure 5 Graphic representation of BIND-014 composed of a biodegradable and hydrophobic PLA polymeric core and a hydrophilic PEG corona decorated with small-molecule (a pseudomimetic PSMA-directed dipeptide) targeting ligands, and a semisynthetic taxane (docetaxel) as an encapsulated anticancer drug.

Note: Images adapted with the permission of BIND Therapeutics (by Gael McGill), Harvard Medical School, and Digizyme Inc.

Abbreviations: PLA, poly(lactic acid); PEG, poly(ethylene glycol); PSMA, prostate-specific membrane antigen.

used cancer chemotherapy drugs.^{127–129} More specifically, a hydrophilic spacer (ie, PEG) was incorporated into the outer shell of the nanoparticle in order to achieve minimal self-self and self-nonself interaction, to escape capture by the reticuloendothelial system, and to reduce opsonization, thus enabling “stealth” properties for immune evasion.^{42,43,130} The tumor-targeting capability of these nanoparticles was obtained by “decorating” the shell surface with RNA A10-aptamer (then replaced with a small molecule urea-based PSMA inhibitor) to bind PSMA.⁴⁰ The biological results demonstrated that the encapsulated drug efficiently interacted with the tumor and selectively delivered docetaxel to prostate cancer cells.^{40,86,87}

Optimization of such construct to BIND-014 was done by adopting a modular self-assembly approach involving use of prefucionalized polymeric materials to generate a combinatorial library of more than 100 self-assembled polymeric targeted nanoparticles of varying composition. This library was designed by introducing physicochemical diversity into each nanoparticle via a focused number of components, and by systematically varying both the nanoformulation and the critical process parameters (Figure 6).¹¹⁶

These targeted docetaxel-loaded nanoparticles were constructed with the above mentioned ternary structure and comprise a biodegradable copolymeric core (PLA or PLGA and PEG), a pseudomimetic dipeptide as a PSMA-targeting ligand, and docetaxel as the payload anticancer drug. Importantly, because scale-up of production for nanoformulations is a huge challenge that has precluded many prototypes going from bench scale experiments to clinical

trials, several key factors that can contribute to the translation of this nanotherapeutic platform were identified. These include the use of FDA-approved polymeric materials that have already been validated for preparation of pharmaceutical products and biomedical application. Moreover, a major goal has been reached by the development of a robust, scalable, and continuous process for efficient nanoparticle formation by using a suitable model (encapsulation of a hydrophobic cancer-preventive compound) to obtain high drug loading and encapsulation efficiency. For example, instantaneous mixing of materials during nanoformulation provides the opportunity to achieve the higher drug loading parameter.¹¹⁶ Therefore, understanding of the fundamental thermodynamics and kinetics to optimize production of the nanoparticles in a repeatable and scalable manner constitutes a key aspect to enable manufacturing of clinical candidate nanoparticles in the kilogram quantities needed for clinical use. The evolution of this process resulted in BIND-014, the first targeted and controlled release polymeric nanoparticle for cancer chemotherapy to reach clinical Phase I trials in January 2011.^{116,131}

Pharmacobiologic profile of BIND-014

Overall, BIND-014 has been demonstrated to be up to 10-fold more effective in delivering docetaxel to tumors with respect to an equivalent dose of free drug in multiple animal models, with no increase in toxicity.¹¹⁶ In particular, as far as tissue biodistribution is concerned, intravenous administration of nanoparticles in *in vivo* experiments in rats showed a blood circulation half-life of about 20 hours,

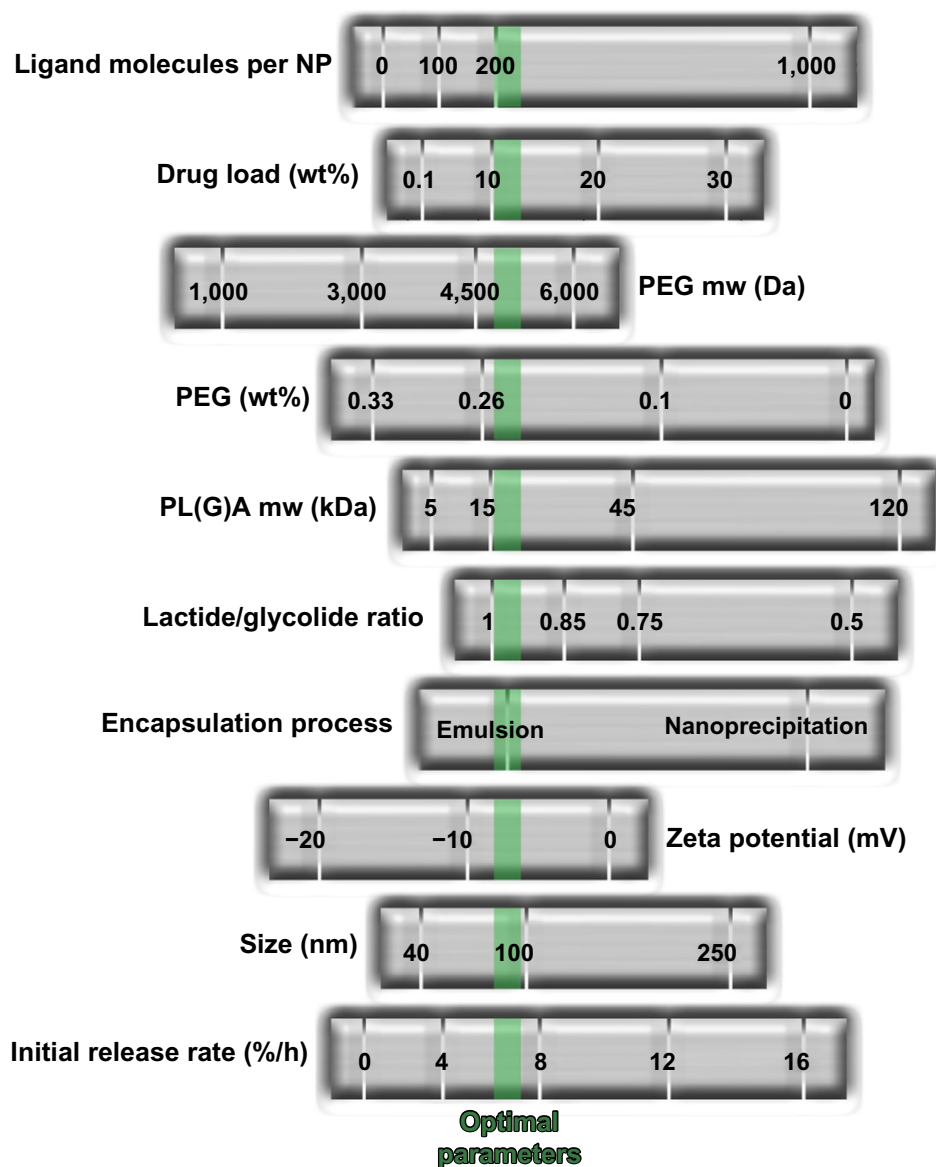


Figure 6 Development of BIND-014 by high-throughput technology. Multifactorial optimization of polymeric nanosystems was performed by varying a range of formulation process parameters and physicochemical nanoparticle properties. The green dotted line indicates optimized nanoparticle parameters.

Notes: Molecular weight expressed in Dalton (Da); zeta potential expressed in millivolts (mV); diameter expressed in nanometers (nm); initial release rate calculated by mass flow per unit time (%/h). From Hrkach J, Von Hoff D, Mukkaram Ali M, et al. Preclinical development and clinical translation of a PSMA-targeted docetaxel nanoparticle with a differentiated pharmacological profile. *Sci Transl Med.* 2012;4(128):128ra139.¹¹⁶ Adapted with permission from AAAS.

Abbreviations: NP, nanoparticles; PEG, poly(ethylene glycol); PL(G)A, poly(lactic acid) or poly(D,L-lactide-co-glycolide).

with higher plasma docetaxel concentrations relative to those of the free drug (as formulated in Taxotere™), where encapsulation prevents rapid distribution of docetaxel from the plasma compartment to tissues (lower accumulation of nanoparticles being detected in liver and bone marrow with respect to plasma). The in vitro release and in vivo pharmacokinetic results also demonstrated that the large amount of docetaxel released from these polymeric nanoprototypes resulted in a long blood circulation time, with sustained release of the drug, leading to an increase of up to 1,000-fold in the docetaxel rate in the plasma, available to

reach tumor sites with respect to the conventional docetaxel formulation (ie, Taxotere).¹¹⁶

Moreover, toxicologic characterization of the composition of free nanoparticles (without drug), targeted nanoparticles, and the respective nontargeted nanoparticles, has been done in a single-dose tolerability study in rats. The results indicated that the ingredients used in the nanoformulation are in general well tolerated, without observation of the hypersensitivity or anaphylactic/anaphylactoid reactions that have been seen after infusion of higher doses of nanoparticles.¹¹⁶

The *in vivo* antitumor activity of the targeted docetaxel-loaded nanoparticles was assessed in mice bearing PSMA-expressing (LNCaP) and PSMA-negative ([breast cancer (MX-1) and nonsmall cell lung cancer (NCI-H460)]) xenograft models, using targeted and nontargeted nanoparticles and free docetaxel for comparison.¹¹⁶ For nanoparticles with a long circulation time, an active targeting mechanism improves antitumor efficacy compared with passive targeting nanoparticles in PSMA-positive models. Mechanistically, once nanoparticles enter the tumor tissue, their retention in tumor tissue and specific uptake by cancer cells can be facilitated by active targeting and receptor-mediated endocytosis. This process would result in higher intracellular drug concentrations and increased cytotoxicity. The similar effects of targeted and nontargeted nanoparticles in non-PSMA-expressing tumors are presumably due to increased drug accumulation at tumor sites via the enhanced permeability and retention effect.

Further, the pharmacokinetic profile of the docetaxel-loaded nanoparticles (compared with that of the free drug) was investigated in tumor-bearing mice, healthy rats, and nonhuman primates to assess the translation of pharmacokinetic results across different species. The results indicate a high concentration of drug in the plasma compartment, as well as an effective controlled drug release performance.¹¹⁶

These preclinical results suggest that nanotherapeutics developed in this way may be beneficial for treatment of solid tumors by improving the therapeutic index of docetaxel through targeting and controlled release of the drug in the tumor microenvironment. Moreover, since the molecular target, PSMA, is expressed on prostate tumor cells and on the neovasculature of other solid tumors, these nanosystems have the potential to increase the utility of docetaxel in the treatment of a range of cancers.

Safety, tolerability, and efficacy of BIND-014 and range of cancer targets

The clinical data for BIND-014 are consistent with the observations outlined above. The behavior of BIND-014 in preclinical studies suggests that docetaxel is more effective when formulated as BIND-014 than as Taxotere. More specifically, on the basis of these promising preclinical results, a Phase I clinical trial was undertaken to assess the dose-limiting toxicity and the maximum tolerated dose of BIND-014.^{116,131} The nanochemotherapy was performed by intravenous infusion of BIND-014 to patients with advanced or metastatic cancer,

using two dosing schedules, ie, once every 3 weeks (Q3W) and once weekly for 3 weeks followed by one week of no treatment over a 4-week cycle (Q1W). To date, BIND-014 has been clinically tested in over 45 patients with advanced or metastatic cancer who have failed prior therapies.

Based on the widespread expression of PSMA in solid tumor neovasculature, the activity of free docetaxel in many common types of cancer, and the efficacy of BIND-014 in preclinical models of prostate and other cancers, a Phase I study was undertaken to evaluate the efficacy of BIND-014 in a panel of solid tumors. It is worth noting that the pharmacokinetics of docetaxel when released from BIND-014 were markedly similar in humans to those observed in preclinical studies, and that the pharmacokinetics of BIND-014 were different from those of Taxotere in both the preclinical and clinical studies. In the Q3W portion of the study, BIND-014 was well tolerated with predictable and manageable toxicities, and no unexpected toxicity has been observed with BIND-014. BIND-014 was demonstrated to be essentially safe and well tolerated, with transient and manageable neutropenia as the dose-limiting toxicity. Other treatment-related adverse events included mild neuropathy, fatigue, mucositis, diarrhea, fluid retention, anemia, rash, hair loss, infusion-related reactions, nail changes, and nausea and vomiting, which are commonly associated with docetaxel as well as many other anticancer drugs.¹³² Further, the maximum tolerated dose was established to be 60 mg/m² as a 60-minute infusion under the Q3W treatment regimen.¹¹⁶ Using this dose regimen, BIND-014 demonstrated antitumor efficacy in nine of 28 patients treated, ranging from one complete response (cervical cancer), three partial responses (non-small-cell lung cancer, metastatic/castration-resistant prostate cancer, and ampullary cancer), and five additional patients with stabilization of disease lasting longer than 12 weeks (pancreatic, colorectal, gallbladder, tonsillar, and anal cancer). These results indicate that the disappearance of cancer evidences in response to treatment, while a partial response refers to a decrease in the size of the tumor or in the extent of cancer in the body.

In summary, the results of a Phase I clinical trial indicate that BIND-014 has a different pharmacologic profile with respect to free docetaxel, including pharmacokinetic properties consistent with a prolonged circulation half-life for BIND-014 and retention of docetaxel in the vascular compartments, with multiple cases of tumor shrinkage at doses up to five times less than the docetaxel dose typically administered.¹³³ These results demonstrate that a combination of long nanoparticle circulation time, nanoparticle targeting, and controlled release of docetaxel

markedly increases the amount of docetaxel delivered to the tumor, and achieves tumor growth inhibition for an extended period of time. Although the Q1W portion of this study is ongoing, Phase II development of BIND-014 as second-line therapy for patients with non-small-cell lung cancer (NCT01792479)¹³⁴ and those with metastatic castrate-resistant prostate cancer (NCT01812746)¹³⁵ was started in 2013 using the Q3W dosing schedule. Further clinical studies to evaluate BIND-014 in a broad range of solid tumors are currently under consideration.

Place in therapy

Nanotechnologies are having a significant impact on drug delivery, and over recent years, several first-generation therapeutic nanoproducts have been moving ahead towards clinical development. In particular, targeted polymeric nanoparticles, capable of increased cell uptake and enhanced accumulation in target tissue, can be successfully obtained by attaching specific binding entities onto the surface of the nanoparticles. Therefore, active targeting, along with other targeting-based approaches, is envisaged to provide an effective strategy, and several ligand-targeted nanotherapeutics are either approved or under clinical evaluation, leading to second-generation nanomedicines. However, although there are many useful and validated chemical methods for functionalizing nanoparticles with a wide range of targeting ligands, several important issues, including the optimal interplay of physicochemical features, need to be addressed before translation from preclinical to clinical development. Importantly, careful detailing of the physicochemical characteristics of nanoparticles that dictate their *in vivo* efficacy and a better understanding of the biological and (patho)physiologic principles of drug targeting are needed to overcome the current bottlenecks in research and development of rationally designed nanoparticles.

The “drug-targeting” paradigm can be exploited to finally formulate therapeutic carriers that can selectively treat neoplastic tissues without affecting normal cells. The use of targeted nanoparticles in the treatment of cancer, developed in the pioneering work of Farokhzad and Langer, has been validated by the Phase II clinically used prototype BIND-014 (marketed by BIND Therapeutics under the brand name Accurins™), a polymeric drug delivery nanovehicle containing the chemotherapeutic agent docetaxel, which is approved for use in the treatment of several common cancers, including breast, lung, and prostate.

To date, other complex targeted nanosystems addressed to various cancers, also combining diagnostic and therapeutic

agents, or that can trigger drug release at the target site when exposed to external stimuli, are currently in clinical development. At this stage, BIND-014 can reasonably be seen as representing an evolution of the “magic bullet” concept, the first description of the drug-targeting paradigm, that can also be used to develop programmable and personalized nanomedicine for routine use in clinic practice.

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Disclosure

The authors report no conflicts of interest in this work.

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