

Evaluation of a minimally invasive procedure for sacroiliac joint fusion – an in vitro biomechanical analysis of initial and cycled properties

Derek P Lindsey¹
 Luis Perez-Orribo²
 Nestor Rodriguez-Martinez²
 Phillip M Reyes²
 Anna Newcomb²
 Alexandria Cable²
 Grace Hickam²
 Scott A Yerby¹
 Neil R Crawford²

¹SI-BONE, Inc., San Jose, CA, USA;
²Spinal Biomechanics Research Laboratory, Barrow Neurological Institute, St Joseph's Hospital and Medical Center, Phoenix, AZ, USA

Introduction: Sacroiliac (SI) joint pain has become a recognized factor in low back pain. The purpose of this study was to investigate the effect of a minimally invasive surgical SI joint fusion procedure on the in vitro biomechanics of the SI joint before and after cyclic loading.

Methods: Seven cadaveric specimens were tested under the following conditions: intact, posterior ligaments (PL) and pubic symphysis (PS) cut, treated (three implants placed), and after 5,000 cycles of flexion–extension. The range of motion (ROM) in flexion–extension, lateral bending, and axial rotation was determined with an applied 7.5 N·m moment using an optoelectronic system. Results for each ROM were compared using a repeated measures analysis of variance (ANOVA) with a Holm–Šidák post-hoc test.

Results: Placement of three fusion devices decreased the flexion–extension ROM. Lateral bending and axial rotation were not significantly altered. All PL/PS cut and post-cyclic ROMs were larger than in the intact condition. The 5,000 cycles of flexion–extension did not lead to a significant increase in any ROMs.

Discussion: In the current model, placement of three 7.0 mm iFuse Implants significantly decreased the flexion–extension ROM. Joint ROM was not increased by 5,000 flexion–extension cycles.

Keywords: biomechanics, iliosacral, arthrodesis, cadaver

Introduction

Low back pain is a significant cause of disability, resulting in 45 million patient visits in 2006.¹ Studies have reported that the sacroiliac (SI) joint is a pain generator in 14.5%–22.5% of patients reporting low back pain.^{2,3} Prior fusion of the lumbar spine is a factor that has exacerbated degeneration of the SI joint in up to 75% patients studied.⁴ As the number of spine fusions continues to grow,¹ it can reasonably be expected that the incidence of SI joint pain will continue to grow.

Until recently, open fusion of the SI joint has been the primary option for SI joint arthrodesis. Recent advances in minimally invasive surgery and medical device technology have allowed for percutaneous fusion of the SI joint. This change to a minimally invasive procedure has led to both greater pain relief and better outcomes.⁵ Additional clinical studies have reported promising results for percutaneous fusion of the SI joint.^{6–11}

One system that allows for a minimally invasive procedure involves placement of a series of triangular implants across the SI joint (iFuse Implant System; SI-BONE, Inc., San Jose, CA, USA). The triangular implants are fabricated out of medical-grade titanium and are coated with a porous titanium plasma spray to allow

Correspondence: Derek P Lindsey
 SI-BONE, Inc., 3055 Olin Avenue,
 Suite 2200, San Jose, CA, USA
 Tel +1 408 207 0700 ext 2245
 Fax +1 408 557 8312
 Email dlindsey@si-bone.com

for biological fixation. The implants are placed to allow for initial mechanical fixation and then rely on biological fixation to permanently stabilize the joint.

Although previous clinical studies have shown promising results, the biomechanics of the initial fixation have not been reported. The objective of this study was to investigate the effects of SI joint fusion on the biomechanics of the SI joint after initial fixation and after 5,000 cycles of flexion–extension.

Methods

Specimen preparation

Eight human cadaveric specimens were used in this study. Specimens were transected rostrally at L4 and included the lower lumbar spine, sacrum, and pelvis. Specimens were obtained fresh frozen and then thawed at room temperature and carefully cleaned of muscle tissue without damaging any ligaments, discs, or joint capsules, including the pubic symphysis. Plain X-ray films were taken to ensure that none of the specimens had any obvious radiographic flaws, visible flaws, or flaws noted on patient history (especially metastatic disease, osteophytes, disc narrowing, or joint arthrosis). Dual energy X-ray absorptiometry (DEXA) scans were performed on the L4 vertebra of each specimen to assess bone mineral density (BMD) and to ensure that none of the specimens had osteoporosis. Specimens were wrapped in plastic bags and stored at -20°C until tested.

On the night before and day of testing, the specimens were thawed for several hours at room temperature while being kept wrapped in saline-soaked gauze. For testing, household screws were inserted into various locations in the exposed L4 endplate and facet articulations, and these screw heads were embedded in fast-curing resin (Smooth Cast 300Q; Smooth-On, Inc., Easton, PA, USA) in a cylindrical potting fixture for application of loads. Similarly, screws were inserted near the right and left ischia on the pelvis and the screw heads were embedded in two separate (right and left) blocks of resin. Each of these resin blocks was of such a shape so that it could be clamped in a vise securely attached to the bottom of the servohydraulic test frame (MTS Systems Corporation, Eden Prairie, MN, USA), while giving free access to instrumentation sites.

Test procedure

The specimens were tested under four conditions: intact, cut posterior ligaments and pubic symphysis, treated, and after 5,000 cycles of flexion and extension.

Under all conditions tested, specimens were studied using standard pure moment flexibility tests in single leg stance. For these tests, an apparatus was used in which a system of cables and pulleys imparts nondestructive, non-constraining torques in conjunction with a standard servohydraulic test system, as described previously.¹² A pure moment is distributed evenly to each motion segment, regardless of the distance from the point of loading.¹³ Moments of 7.5 N·m maximum were applied about the appropriate anatomical axes to induce three different types of motion: flexion–extension, lateral bending, and axial rotation. Single leg stance was modeled by clamping the resin block attached to the ipsilateral acetabulum in the vise and letting the resin block attached to the acetabulum on the contralateral side hang freely (Figure 1). All range of motions (ROMs) were calculated using a motion analysis system and custom software (as detailed below).

After completion of testing the intact condition, a simulated instability was used to reduce the stability of the SI joint. This reduction was accomplished by sectioning the

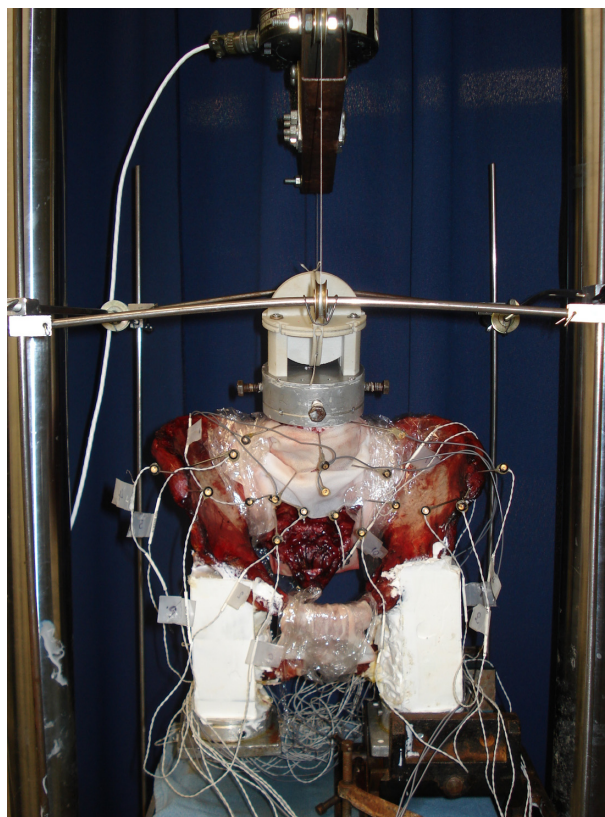


Figure 1 Photograph of the experimental test setup as configured for flexion testing. **Notes:** Pure moments are applied to the specimen using the circular fixture attached to L4 with cable tension supplied by the materials testing system. Note how the resin block attached to the left acetabulum is clamped in a vise that is rigidly attached to the bottom of the test frame to simulate single leg stance. The resin block on the contralateral acetabulum was allowed to hang freely. Optical markers were attached to L4, L5, sacrum (two locations), left ilium, and right ilium to track three-dimensional motion.

posterior ligaments (including the capsule) and the pubic symphysis. The loading protocol was repeated and the ROMs were calculated for the reduced stability condition.

For the treated condition, all implants (iFuse Implant 7.0 mm; SI-BONE, Inc.) were placed according to the manufacturer's recommendations. Briefly, the implants were placed using a pin, drill, broach, and implant methodology. A guide pin was placed under fluoroscopic guidance using the appropriate views (lateral, inlet, and outlet). The length of the implant was measured after placement of the pin. Next, a drill was used to prepare a hole that was broached to allow for placement of the implant. The second and third implants were placed parallel to the initial implant and approximately parallel to the posterior wall of the spinal canal (Figure 2). After treatment was completed, the ROMs were determined using the previously defined loading protocol.

To determine the cyclic stability of the treated specimens, 5,000 cycles of flexion and extension were applied. The peak moment for cyclic loading varied between 3.75 and 7.5 N·m (Table 1). After cyclic loading was completed, the loading protocol was repeated and ROMs calculated.

Motion analysis

Three-dimensional specimen motion in response to the applied loads during flexibility tests was determined using the Optotrak 3020 system (Northern Digital, Waterloo, ON, Canada). This system stereophotogrammetrically measures the three-dimensional displacement of infrared-emitting markers rigidly attached in a non-collinear arrangement to six regions on the lumbar spine and pelvic ring, including L4, L5, the sacrum (two locations), and the right and left ilia. Custom software converts the marker coordinates to angles about each of the anatomical axes in terms of the motion segment's own coordinate system.¹⁴ The coordinate system for each pair of marker triads was aligned to the anatomy of L5, with the lateral axis (*x*) aligned with points near the intersection of the pedicle and vertebral body, and the antero-posterior (*z*) axis aligned by interconnecting a midsagittal point at the anterior base of the L5 vertebral body to a point on the spinous process (this vector was aligned by eye to the L5–S1 rostral endplate). Spinal angles were calculated using a technique that provides appropriate results for describing three-dimensional spinal motion.¹⁵

Data analysis

From the data, the angular ROM was generated. Analysis was performed on raw values (in degrees) or normalized values.

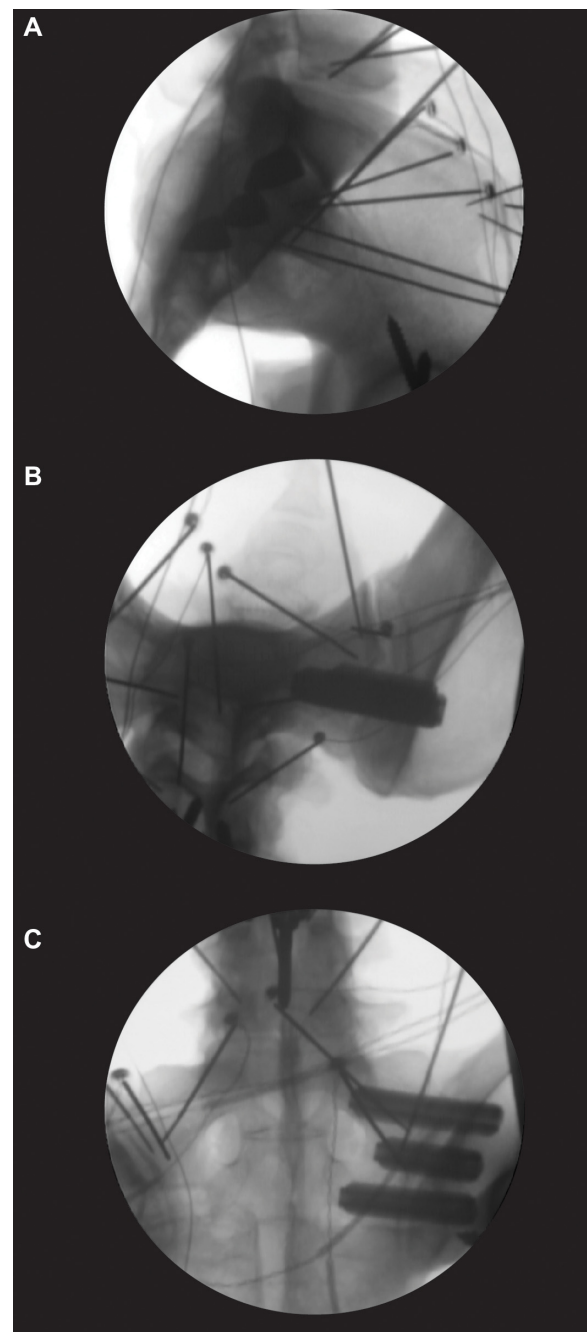


Figure 2 Representative fluoroscopic images showing placement of the three 7.0 mm implants placed in the (A) lateral, (B) inlet, and (C) outlet views.

Note: The wires and pins supporting the infrared LED markers for the tracking system are visible in the radiographs.

Abbreviation: LED, light-emitting diode.

Statistical comparisons were made with SigmaPlot (v12.5; Systat Software, Inc., San Jose, CA, USA).

A repeated measures analysis of variance (ANOVA) was used to analyze the outcomes between treatments. Post-cyclic values from the three peak moments were pooled for the repeated measures ANOVA. A Holm–Šidák post-hoc test was used to determine significant differences between

Table 1 Specimen information and testing parameters

Specimen	Sex	Age (years)	L4 DEXA (BMD g/cm ²)	Side tested	Maximum cyclic moment (N·m)
SI03	M	64	0.685	Left	7.5
SI04	F	60	0.669	Right	7.5
SI05	F	59	0.711	Left	3.75
SI06	F	52	1.114	Right	3.75
SI08	M	49	0.899	Right	5.625
SI09	M	65	1.166	Left	5.625
SI10	F	64	0.574	Left	5.625
SI11	F	55	0.666	–	–
*Mean ± SD		59±6.3	0.831±0.233		

Note: *Mean and SD excludes specimen SI11, which deteriorated during testing.

Abbreviations: BMD, bone mineral density; DEXA, dual energy X-ray absorptiometry; SD, standard deviation.

groups. Linear regression was used to analyze the correlation between the maximum moment and change in normalized ROM. *P*-values less than 0.05 were considered significant.

Results

Seven specimens completed the testing (Table 1). One specimen (SI11) deteriorated during testing and was unable to complete the testing protocol; it was not included in the subsequent analysis.

Sectioning of the posterior ligaments and pubic symphysis resulted in significant increases in flexion–extension ($P<0.001$), lateral bending ($P<0.001$), and axial rotation ROMs ($P<0.001$) (Table 2 and Figure 3). Placement of the implants led to a significant decrease from the cut condition in flexion–extension ($P=0.045$), but not lateral bending ($P=0.083$) or axial rotation ROM ($P=0.058$). Cyclic loading of the specimens did not result in any significant changes from the implanted condition for flexion–extension ($P=0.403$), lateral bending ($P=0.408$), or axial rotation ($P=0.697$).

The correlations between the maximum moment during cyclic loading and the change in the ROM between implanted and post-cyclic samples were not significant for flexion–extension ($P=0.435$), lateral bending ($P=0.466$), or axial rotation ($P=0.816$; Figure 4).

Discussion

The in vitro biomechanical model here presents ROM data that is consistent with previous clinical studies.^{16–19} In the current study, it was found that in the intact condition, the magnitude of SI joint motion that occurred normally was largest in flexion–extension (2.3°), then axial rotation (1.7°), and smallest in lateral bending (1.1°). Egund et al found in an examination of four patients presenting with low back pain that testing with symmetric forces typically rotated the sacrum around the transverse axis up to 2°.¹⁶ Stuesson et al investigated 25 symptomatic patients aged 18–45 years and found flexion–extension rotations ranging from 0.6° to 3.6°.¹⁷ Jacob and Kissling investigated healthy individuals

Table 2 Sacroiliac joint ROM testing results for seven specimens

Specimen	Side	Sacroiliac joint ROM (degrees)											
		Flexion–extension				Lateral bending				Axial rotation			
		Intact	PL and PS cut	Treated	Post-cyclic	Intact	PL and PS cut	Treated	Post-cyclic	Intact	PL and PS cut	Treated	Post-cyclic
SI03	L	1.54	9.29	6.38	10.26	0.66	4.75	3.67	4.72	1.2	10.21	7.31	9.47
SI04	R	5.12	9.59	7.45	7.84	2.86	5.72	3.76	4.4	3.31	6.8	6.08	4.68
SI05	L	2.49	7.45	3.18	3.56	1.26	3.36	1.72	2.12	1.73	5.95	3.65	3.33
SI06	R	2.14	9.17	1.57	1.71	0.58	3.59	0.81	0.81	1.05	6.12	3.69	3.85
SI08	R	0.99	2.7	2.85	3.64	0.45	1.55	1.71	2.06	1.02	3.2	2.92	3.47
SI09	L	1.61	3.15	2.25	1.69	0.72	1.31	0.97	0.9	1.73	3.6	1.56	2.09
SI10	L	2.01	7.3	6.33	6.97	1.06	2.66	3.24	3.38	1.65	9.41	6.88	7.25
Mean		2.27	6.95	4.29	5.10	1.08	3.28	2.27	2.63	1.67	6.47	4.58	4.88
SD		1.35	2.89	2.36	3.30	0.83	1.61	1.26	1.58	0.79	2.65	2.18	2.58

Notes: Specimens were tested in flexion–extension, lateral bending, and axial rotation using a 7.5 N·m test moment. Treatments include intact, PL and PS cut, placement of three 7.0 mm iFuse Implants (treated), and after 5,000 cycles of flexion–extension loading (post-cyclic).

Abbreviations: PL, posterior ligaments; PS, pubic symphysis; ROM, range of motion; SD, standard deviation.

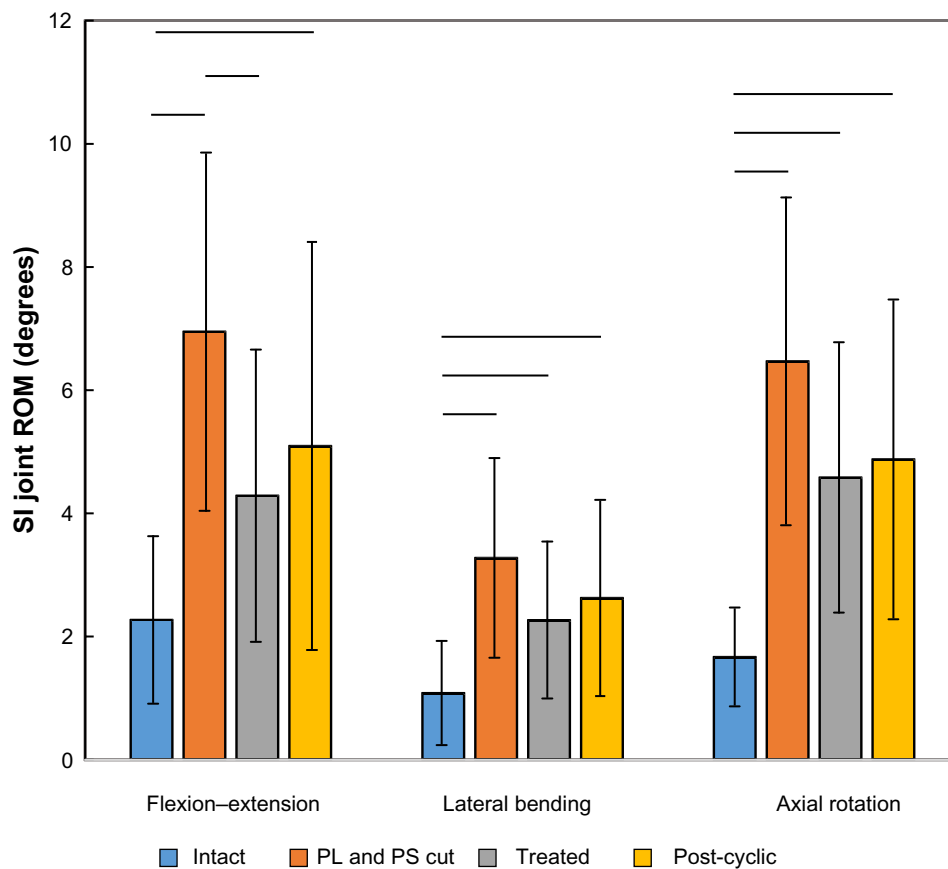


Figure 3 Flexion–extension, lateral bending, and axial rotation ROM data for seven SI joint specimens tested with pure moment loading.

Notes: Treatments include intact, PL and PS cut, placement of three implants (treated), and after 5,000 cycles of flexion–extension loading (post-cyclic). Data presented as mean \pm SD. Lines denote statistically significant differences ($P < 0.05$).

Abbreviations: PL, posterior ligaments; PS, pubic symphysis; ROM, range of motion; SD, standard deviation; SI, sacroiliac.

20–50 years of age and found flexion–extension rotations from 0° up to 4.4° .¹⁸ Stuesson et al also investigated six female patients aged 28–35 years with pelvic pain and found that hyperextension of the leg could lead to flexion–extension values up to 3.9° .¹⁹ These studies consistently report that the ROM is largest in flexion–extension, then axial rotation, and smallest in lateral bending.^{17–19}

A direct comparison of angles measured here to those from previous in vitro studies is not possible because other researchers did not quantify angular ROM in response to loads intended to produce planar rotational responses or use pure moments. Typical tests in prior in vitro studies ignored bending (or measured only slight bending secondary to compression).^{20–23} Other studies have applied offset compression to induce bending.^{24,25} A few studies have included pure moments in conjunction with follower loads to analyze the motion of the SI joint.^{26–28} The use of a follower load is thought to stabilize the spine, although its appropriateness is debated. By not including a follower load, the accuracy and consistency of the pure moment loading can be assured.

Cutting the posterior ligaments and pubic symphysis led to significant increases of flexion–extension, lateral bending, and axial rotation. The sectioning of these led to values that are consistent with those reported for motions reported with extreme hip positions in normal cadaver joints.²⁹ One concern was that this destabilization of the joint may lead to further degradation. Although one specimen did degrade, seven of the specimens continued to be stable and allowed for testing of the fusion devices and subsequent cyclic testing.

Placement of the fusion devices led to a significant decrease in flexion–extension. As previously detailed, flexion–extension is the dominate motion of the SI joint for the given loads. Reduction in joint motion is the primary goal and keeping this reduction will likely improve biological fixation. Although not significant, lateral bending was decreased in five out of seven specimens and axial rotation was decreased in all specimens, suggesting that the implants are effective in a large percentage of specimens. The cause of the increase in lateral bending in two out of seven specimens is unclear and is of interest for further investigation.

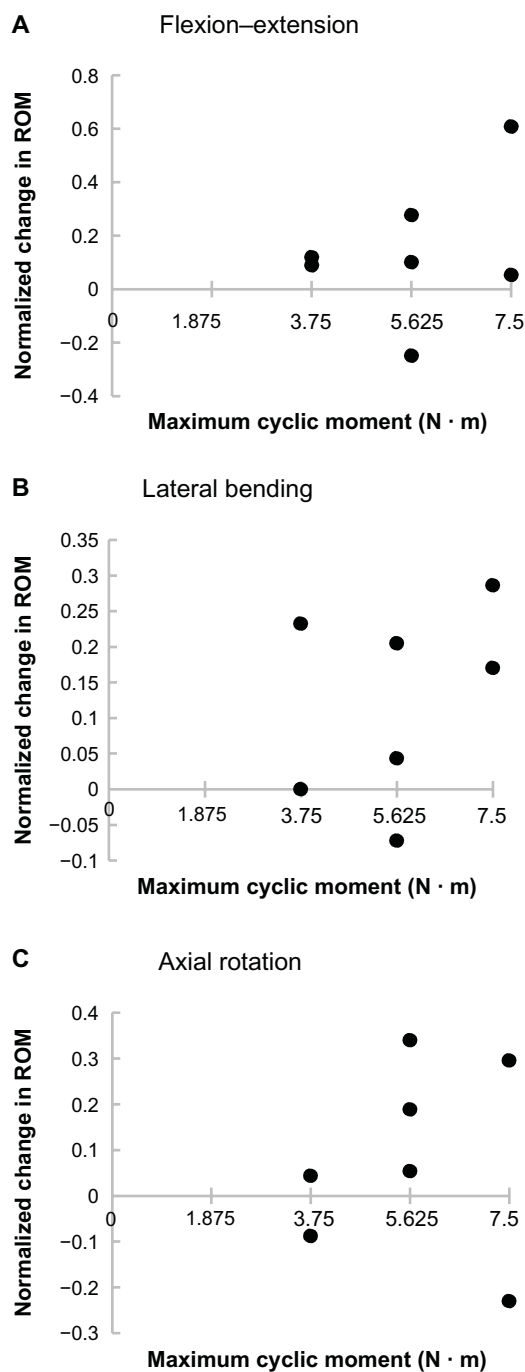


Figure 4 Normalized change in the SI joint ROM after 5,000 flexion–extension loading cycles as a function of maximum cyclic moment for (A) flexion–extension, (B) lateral bending, and (C) axial rotation.

Notes: All ROM data were normalized using the following equation: (post-cyclic – treated)/(treated). No correlations between maximum moment and normalized change in ROM were significant ($P < 0.05$).

Abbreviations: ROM, range of motion; SI, sacroiliac.

Cyclic loading of the treated SI joint did not lead to any significant changes in flexion–extension, lateral bending, or axial rotation ROMs. For the tested maximum moments, this suggests that no loosening of the SI joint was observed. Extrapolation of the cyclic results to the clinical condition

must be made with caution. As with all in vitro models, it is not possible to investigate the results that the biological response will have on the stability of the treated SI joint.

The current study is not without limitations. The investigated model included sectioning of the posterior ligaments and the pubic symphysis. This study was set up to investigate a single SI joint and the effects of a fusion procedure on that joint. As such, the model in this investigation does not purely reflect the clinical condition as the pubic symphysis would likely be repaired. The resulting ROM data here are larger than the condition with the pubic symphysis intact. Although that model does warrant further investigation, the authors believe that the results of this study will translate to that condition.

Conclusion

The use of pure-moments in the reported pelvic model produced flexion–extension, lateral bending, and axial rotation SI joint ROMs that are consistent with previous clinical results. Simulated instability of the posterior ligaments and pubic symphysis led to significantly increased ROMs. After simulating an instability, placement of three SI fusion devices significantly reduced the flexion–extension ROM. Post-implantation cyclic loading did not result in any significant ROM changes in flexion–extension, lateral bending, or axial rotation. The use of the tested fusion devices provided for a more stable construct that did not significantly degrade during cyclic loading.

Disclosure

This study was funded by SI-BONE, Inc., Derek P Lindsey and Scott A Yerby are SI-BONE, Inc., employees. Neil R Crawford received research grant support (paid directly to the institution) from SI-BONE, Inc. The authors have no other conflicts of interest to report in this work.

References

1. United States Bone and Joint Initiative. *The Burden of Musculoskeletal Diseases in the United States*. 2nd ed. Rosemont, IL: American Academy of Orthopedic Surgeons; 2011.
2. Sembrano JN, Polly DW Jr. How often is low back pain not coming from the back? *Spine (Phila Pa 1976)*. 2009;34(1):E27–E32.
3. Bernard TN Jr, Kirkaldy-Willis WH. Recognizing specific characteristics of nonspecific low back pain. *Clin Orthop Relat Res*. 1987;(217): 266–280.
4. Ha KY, Lee JS, Kim KW. Degeneration of sacroiliac joint after instrumented lumbar or lumbosacral fusion: a prospective cohort study over five-year follow-up. *Spine (Phila Pa 1976)*. 2008;33(11):1192–1198.
5. Smith AG, Capobianco R, Cher D, et al. Open versus minimally invasive sacroiliac joint fusion: a multi-center comparison of perioperative measures and clinical outcomes. *Ann Surg Innov Res*. 2013;7(1):14.
6. Al-Khayer A, Hegarty J, Hahn D, Grevitt MP. Percutaneous sacroiliac joint arthrodesis: a novel technique. *J Spinal Disord Tech*. 2008;21(5): 359–363.

7. Cummings J Jr, Capobianco RA. Minimally invasive sacroiliac joint fusion: one-year outcomes in 18 patients. *Ann Surg Innov Res*. 2013;7(1):12.
8. Rudolf L. Sacroiliac joint arthrodesis-MIS technique with titanium implants: report of the first 50 patients and outcomes. *Open Orthop J*. 2012;6:495–502.
9. Duhon BS, Cher DJ, Wine KD, Lockstadt H, Kovalsky D, Soo CL. Safety and 6-month effectiveness of minimally invasive sacroiliac joint fusion: a prospective study. *Med Devices (Auckl)*. 2013;6:219–229.
10. Mason LW, Chopra I, Mohanty K. The percutaneous stabilisation of the sacroiliac joint with hollow modular anchorage screws: a prospective outcome study. *Eur Spine J*. 2013;22(10):2325–2331.
11. Sachs D, Capobianco R. Minimally invasive sacroiliac joint fusion: one-year outcomes in 40 patients. *Adv Orthop*. 2013;2013:536128.
12. Crawford NR, Brantley AG, Dickman CA, Koeneman EJ. An apparatus for applying pure nonconstraining moments to spine segments in vitro. *Spine (Phila Pa 1976)*. 1995;20(19):2097–2100.
13. Panjabi MM. Biomechanical evaluation of spinal fixation devices: I. A conceptual framework. *Spine (Phila Pa 1976)*. 1988;13(10):1129–1134.
14. Crawford NR, Dickman CA. Construction of local vertebral coordinate systems using a digitizing probe. Technical note. *Spine (Phila Pa 1976)*. 1997;22(5):559–563.
15. Crawford NR, Yamaguchi GT, Dickman CA. A new technique for determining 3-D joint angles: the tilt/twist method. *Clin Biomech (Bristol, Avon)*. 1999;14(3):153–165.
16. Egund N, Olsson TH, Schmid H, Selvik G. Movements in the sacroiliac joints demonstrated with roentgen stereophotogrammetry. *Acta Radiol (Stockh)*. 1978;19(5):833–846.
17. Stuesson B, Selvik G, Udén A. Movements of the sacroiliac joints. A roentgen stereophotogrammetric analysis. *Spine (Phila Pa 1976)*. 1989;14(2):162–165.
18. Jacob HA, Kissling RO. The mobility of the sacroiliac joints in healthy volunteers between 20 and 50 years of age. *Clin Biomech (Bristol, Avon)*. 1995;10(7):352–361.
19. Stuesson B, Uden A, Vleeming A. A radiostereometric analysis of the movements of the sacroiliac joints in the reciprocal straddle position. *Spine (Phila Pa 1976)*. 2000;25(2):214–217.
20. Dujardin FH, Roussignol X, Hossenbaccus M, Thomine JM. Experimental study of the sacroiliac joint micromotion in pelvic disruption. *J Orthop Trauma*. 2002;16(2):99–103.
21. Schildhauer TA, Ledoux WR, Chapman JR, Henley MB, Tencer AF, Routt ML Jr. Triangular osteosynthesis and iliosacral screw fixation for unstable sacral fractures: a cadaveric and biomechanical evaluation under cyclic loads. *J Orthop Trauma*. 2003;17(1):22–31.
22. Sagi HC, Ordway NR, DiPasquale T. Biomechanical analysis of fixation for vertically unstable sacroiliac dislocations with iliosacral screws and symphyseal plating. *J Orthop Trauma*. 2004;18(3):138–143.
23. Mears SC, Sutter EG, Wall SJ, Rose DM, Belkoff SM. Biomechanical comparison of three methods of sacral fracture fixation in osteoporotic bone. *Spine (Phila Pa 1976)*. 2010;35(10):E392–E395.
24. Wood KB, Schendel MJ, Ogilvie JW, Braun J, Major MC, Malcom JR. Effect of sacral and iliac instrumentation on strains in the pelvis. A biomechanical study. *Spine (Phila Pa 1976)*. 1996;21(10):1185–1191.
25. Kim JH, Horton W, Hamasaki T, Freedman B, Whitesides TE Jr, Hutton WC. Spinal instrumentation for sacral-pelvic fixation: a biomechanical comparison between constructs ending with either S2 bicortical, bitriangulated screws or iliac screws. *J Spinal Disord Tech*. 2010;23(8):506–512.
26. Shaw JA, Mino DE, Werner FW, Murray DG. Posterior stabilization of pelvic fractures by use of threaded compression rods. Case reports and mechanical testing. *Clin Orthop Relat Res*. 1985;(192):240–254.
27. Comstock CP, van der Meulen MC, Goodman SB. Biomechanical comparison of posterior internal fixation techniques for unstable pelvic fractures. *J Orthop Trauma*. 1996;10(8):517–522.
28. Yu B, Zheng Z, Zhuang X, et al. Biomechanical effects of transverse partial sacrectomy on the sacroiliac joints: an in vitro human cadaveric investigation of the borderline of sacroiliac joint instability. *Spine (Phila Pa 1976)*. 2009;34(13):1370–1375.
29. Smidt GL, Wei SH, McQuade K, Barakatt E, Sun T, Stanford W. Sacroiliac motion for extreme hip positions. A fresh cadaver study. *Spine (Phila Pa 1976)*. 1997;22(18):2073–2082.

Medical Devices: Evidence and Research

Publish your work in this journal

Medical Devices: Evidence and Research is an international, peer-reviewed, open access journal that focuses on the evidence, technology, research, and expert opinion supporting the use and application of medical devices in the diagnosis, treatment and management of clinical conditions and physiological processes. The identification of novel

Submit your manuscript here: <http://www.dovepress.com/medical-devices-evidence-and-research-journal>

Dovepress

devices and optimal use of existing devices which will lead to improved clinical outcomes and more effective patient management and safety is a key feature. The manuscript management system is completely online and includes a quick and fair peer-review system. Visit <http://www.dovepress.com/testimonials.php> to read real quotes from authors.