

# The digital aqueous humor outflow meter: an alternative tool for screening of the human eye outflow facility

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Vassilios P Kozobolis  
Eleftherios I Paschalis  
Nikitas C Foudoulakis  
Stavrenia C Koukoulas  
Georgios Labiris

Department of Ophthalmology and  
Eye Institute of Thrace, Democritus  
University of Thrace, Alexandroupolis,  
Greece

**Purpose:** To develop, characterize, and validate a prototype digital aqueous humor outflow tonographer (DAHOM).

**Material and methods:** The DAHOM was developed, characterized, and validated in three phases. Phase 1 involved construction of the sensor. This was broadly based on the fundamental design of a typical Schiottz tonographer with a series of improvements, including corneal indentation, which was converted to an electrical signal via a linear variable differential transducer, an analog signal which was converted to digital via ADC circuitry, and digital data acquisition and processing which was made possible by a serial port interface. Phase 2 comprised development of software for automated assessment of the outflow facility. Automated outflow facility assessment incorporated a series of fundamental improvements in comparison with traditional techniques, including software-based filtering of ripple noise and extreme variations, rigidity impact analysis, and evaluation of the impact of patient age, central corneal thickness, and ocular axial length. Phase 3 comprised characterization and validation of DAHOM, for which we developed an experimental setup using porcine cadaver eyes. DAHOM's repeatability was evaluated by means of Cronbach's alpha and intraclass correlation coefficient. The level of agreement with a standard Schiottz tonographer was evaluated by means of paired *t*-tests and Bland-Altman analysis in human eyes.

**Results:** The experimental setup provided the necessary data for the characterization of DAHOM. A fourth order polynomial equation provided excellent fit ( $R^2 > 0.999$ ). DAHOM demonstrated high repeatability (Cronbach's alpha  $\geq 0.997$ ; intraclass correlation coefficient  $\geq 0.987$ ) and an adequate level of agreement with a standard Schiottz tonographer.

**Conclusions:** This study presents the development, characterization, and validation of a prototype digital tonographer. DAHOM demonstrates high repeatability and a sufficient level of agreement with a typical Schiottz tonographer, while its digital design remedies known vulnerabilities of conventional tonographers.

**Keywords:** glaucoma, tonography, pressure, outflow facility, aqueous humor

## Introduction

The importance of aqueous humor tonography in research settings has been highlighted over many years.<sup>1-3</sup> Tonography outcomes provide essential information for a series of ophthalmic diseases, eg, the glaucomas, and facilitate exploration of the ocular manifestations of systemic diseases. However, tonography in daily clinical settings has yet to be applied, mainly due to time constraints in hospital departments. Moreover, prevalent tonographic settings suffer from poor repeatability which limits their clinical usefulness. Among the primary causes of variability is the fact that reliable measurements require continuous eye alignment, which is

Correspondence: Eleftherios Paschalis Ilios  
Eye Institute of Thrace, University  
Hospital of Alexandroupolis,  
68 100 Dragana, Alexandroupolis,  
Thrace, Greece  
Tel +30 255 107 6109  
Fax +30 281 030 359  
Email epaschalis@hotmail.com

difficult to achieve in practice. On the other hand, data collection and processing using traditional tonographers is difficult, because they do not provide digital output, automated assessment of the outflow facility, or evaluation of the impact of a series of known modifiers of the outflow facility. Within this context, we demonstrate here the development, characterization, and validation of a novel digital aqueous humor outflow topographer (DAHOM) that addresses the series of vulnerabilities of traditional tonographers.

## Materials and methods

### Setting

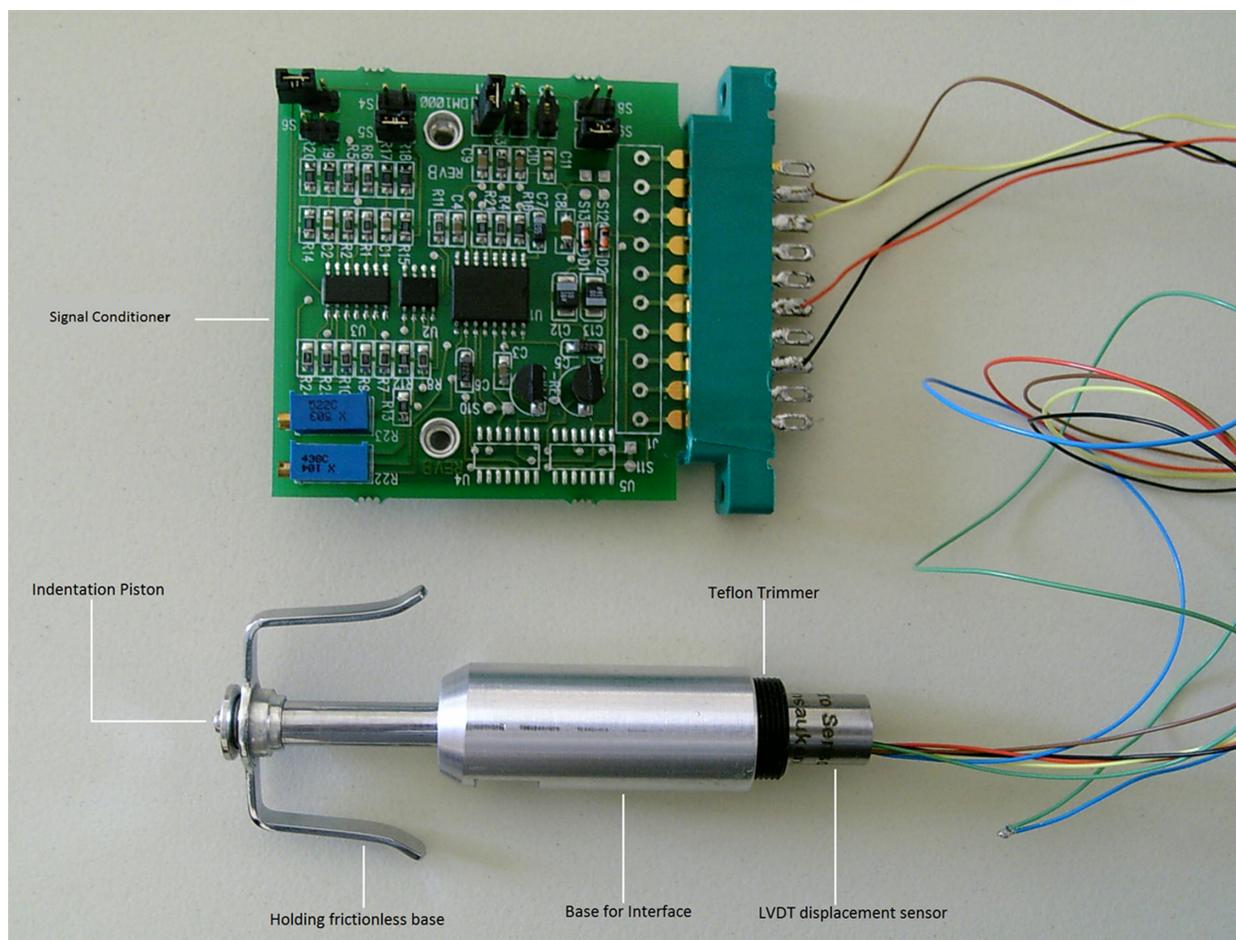
The study adhered to the tenets of the Declaration of Helsinki and written informed consent was given by all participants. This was a prospective study conducted in the Department of Ophthalmology at the University Hospital of Alexandroupolis in Greece between 2004 and 2007.

## Development of DAHOM

The digital outflow meter was designed at the Eye Institute of Thrace, in collaboration with the Electrical Engineering Department of the Technical University of Thrace. The development of the system was done in three phases.

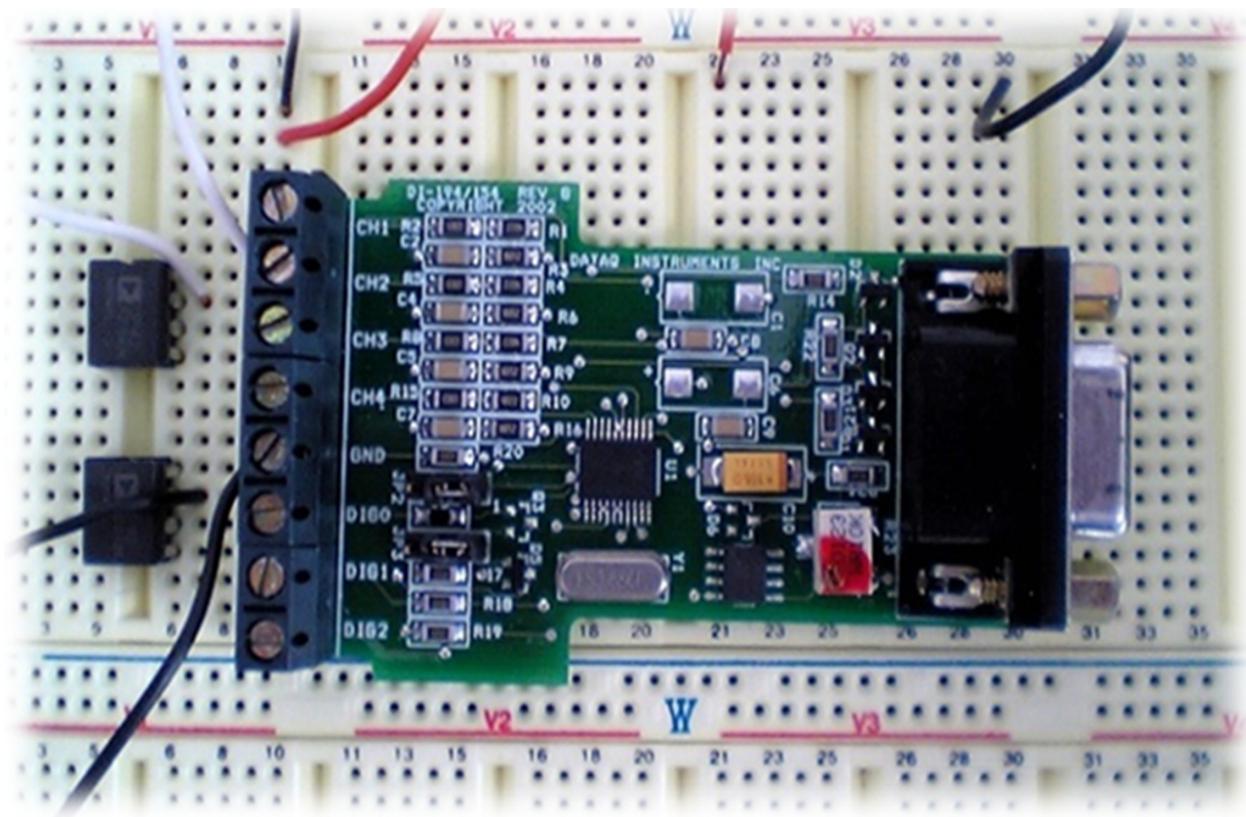
### Phase I

Phase I included construction of the electromechanical system with the sensor and the electronic circuitry (Figure 1). The sensor design was broadly based on the fundamental design of a typical Schiøtz tonographer. The sensor converted corneal indentation to electrical signal with high sensitivity ( $1.719 \text{ mV/volt}/0.0254 \text{ mm}$ ) using a linear variable differential transducer. All elements were connected to an aluminum alloy frame capable of retraction and sterilization. Analog to digital signal conversion was accomplished using ADC electronic circuitry providing interface via a serial port (RS232, Figure 2).



**Figure 1** Digital outflow meter, including linear variable differential transducer and signal conditioner circuit.

The digital outflow transducer with the contact tip (indentation piston), the base (center), and the linear variable differential transducer sensor (right). Connector cables are used for power supply and data transfer to the DAQ board. The signal conditioning board is responsible for sinusoidal wave generation, signal rectification, and phase-sensitive demodulation processing.



**Figure 2** Data acquisition board with analog to digital converter and serial communication with a PC. Electronic circuitry with data acquisition, analog to digital converter, and RS 232 communication interface.

### Phase 2

Phase 2 involved development of the software and the conversion algorithm for the evaluation of the outflow facility. A software-based percentile filter was used to cut out ripple noise and random measurement variations (Figure 3). Observed differences in intraocular pressure (IOP) measurements between the DAHOM and Goldmann applanation tonometer (GAT) were used for assessment of ocular rigidity.

The outflow facility was calculated according to the following formula:

$$C_{out} = \frac{\Delta V}{\left(\frac{P_{t0} + P_{t4}}{2} - P_{applanation} - \Delta P_{indentation}\right) \cdot 4}$$

$$= \frac{(V_{C4} - V_{C0}) + \frac{1}{K} \log\left(\frac{P_{t0}}{P_{t4}}\right)}{\left(\frac{P_{t0} + P_{t4}}{2} - P_{applanation} - \Delta P_{indentation}\right) \cdot 4}$$

where  $V_{C4} - V_{C0}$  is the corneal volume displacement during the tonography study, K is the sclera rigidity factor or ocular rigidity factor,  $P_{t0}/P_{t4}$  is the hydrostatic pressure difference

between the points of flow resistance,  $P_{applanation}$  is the IOP measured by GAT,  $\Delta P$  is the mechanical increase of IOP from the weight of the tonographer, and 4 is duration of the study in minutes.<sup>4</sup>

A software program was developed in Java language, capable of calculating the outflow facility (Figure 4). Rigidity impact analysis was incorporated in the software algorithm using GAT IOP measurement, as suggested by Friedenwald.<sup>4</sup>

The following formula was used to calculate rigidity:

$$Rigidity = 4.5282E^{-5} + 6.7443E^{-4}X + 6.165E^{-6}X^2$$

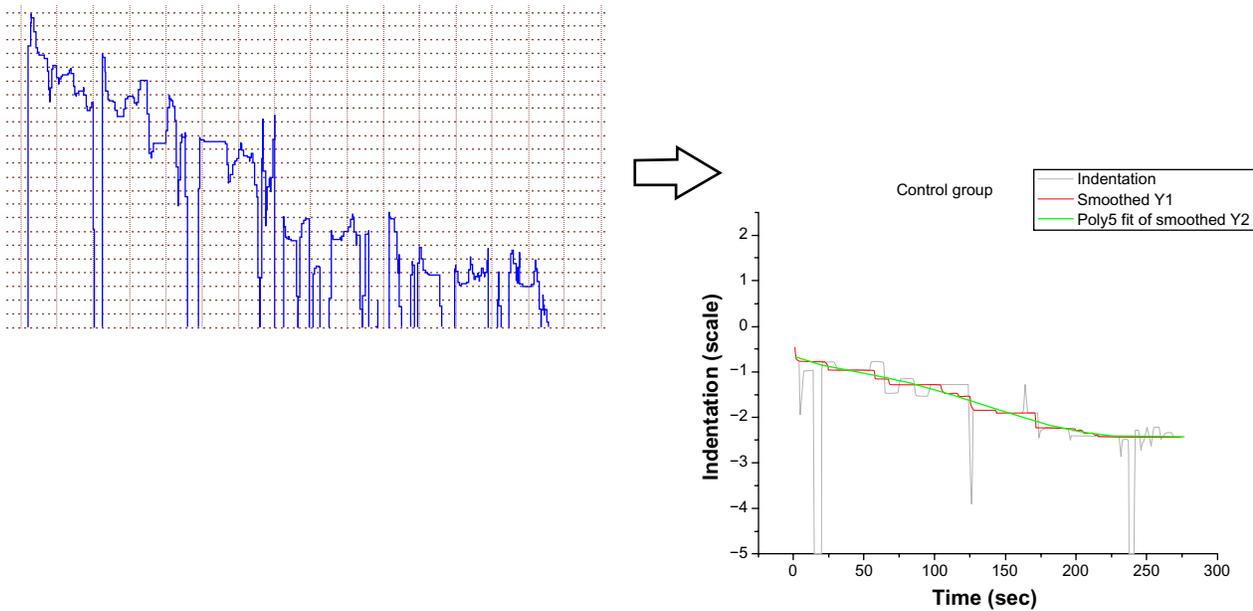
$$- 2.18104E^{-7}X^3 - 2.07212E^{-8}X^4 + 2.7598E^{-9}X^5$$

$$- 1.1391E^{-10}X^6 + 2.26627E^{-12}X^7$$

$$- 2.20326E^{-14}X^8 + 8.45107E^{-17}X^9$$

where X is the mathematical arc tangent operator of the difference between the applanation and the indentation IOP, while the following three formulas (F1–F3) were used to define the indentational versus IOP measurement for 5.5, 7.5, and 10 g weight of the digital outflow meter:

$$IOP_{indent}^{5.5g} = 51.081 - 5.887x + 0.479x^2 - 0.0215x^3 + 3.832E^{-4}x^4 \tag{F1}$$



**Figure 3** Data filtering and tonographic polynomial fit. Data as recorded in real time by the data acquisition system (left graph) and data post-study analysis with digital filtering (red line) and polynomial fit (green line, right graph).

$$IOP_{indent}^{7.5g} = 69.668 - 8.045x + 0.655x^2 - 0.029x^3 + 5.204E^{-4}x^4 \quad (F2)$$

$$IOP_{indent}^{10g} = 92.89 - 10.717x + 0.872x^2 - 0.039x^3 + 6.937E^{-4}x^4 \quad (F3)$$

where  $x$  is the magnitude of indentation for the digital tonographer in mm.

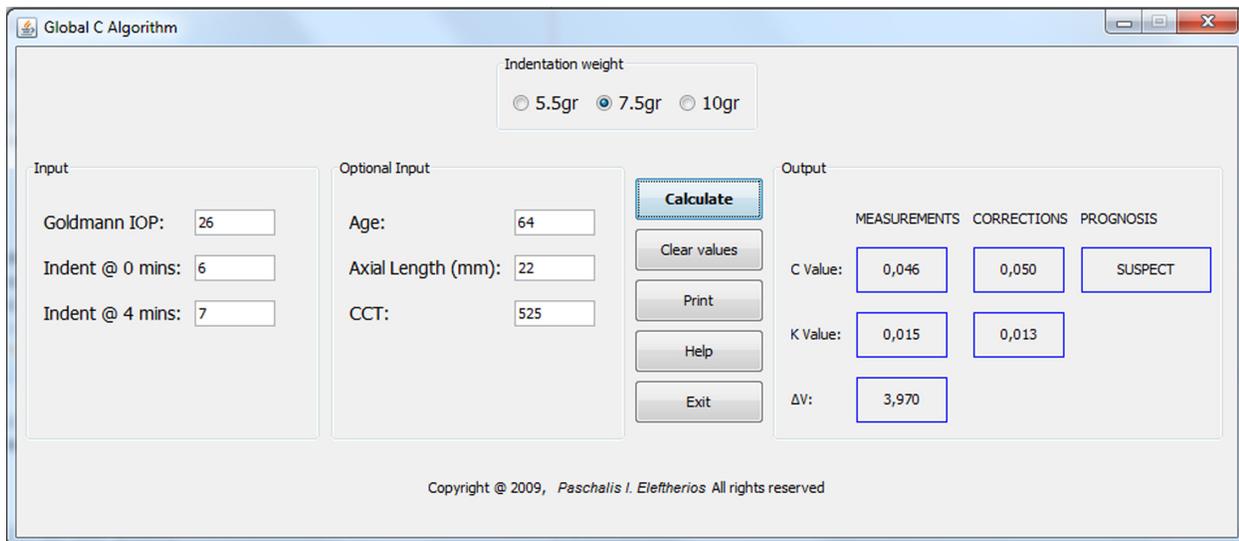
A series of optional parameters were also incorporated in the algorithm in order to correct the rigidity measurements

based on the influence of several biomechanical factors, including central cornea thickness, age of patient, and ocular axial length (Figure 4). These formulae were derived from previously published studies on ocular rigidity variation.<sup>5,6</sup>

$$K_{age} = 0.00526 + 1.09285E^{-4} \times Age$$

$$K_{cct} = -0.02055 + 6.33781E^{-5} \cdot CCT$$

$$K_{refraction} = 0.02056 + 6.6158E^{-4}L + 2.0559E^{-5}L^2 + 9.70044E^{-7}L^3 + 1.6981E^{-8}L^4$$



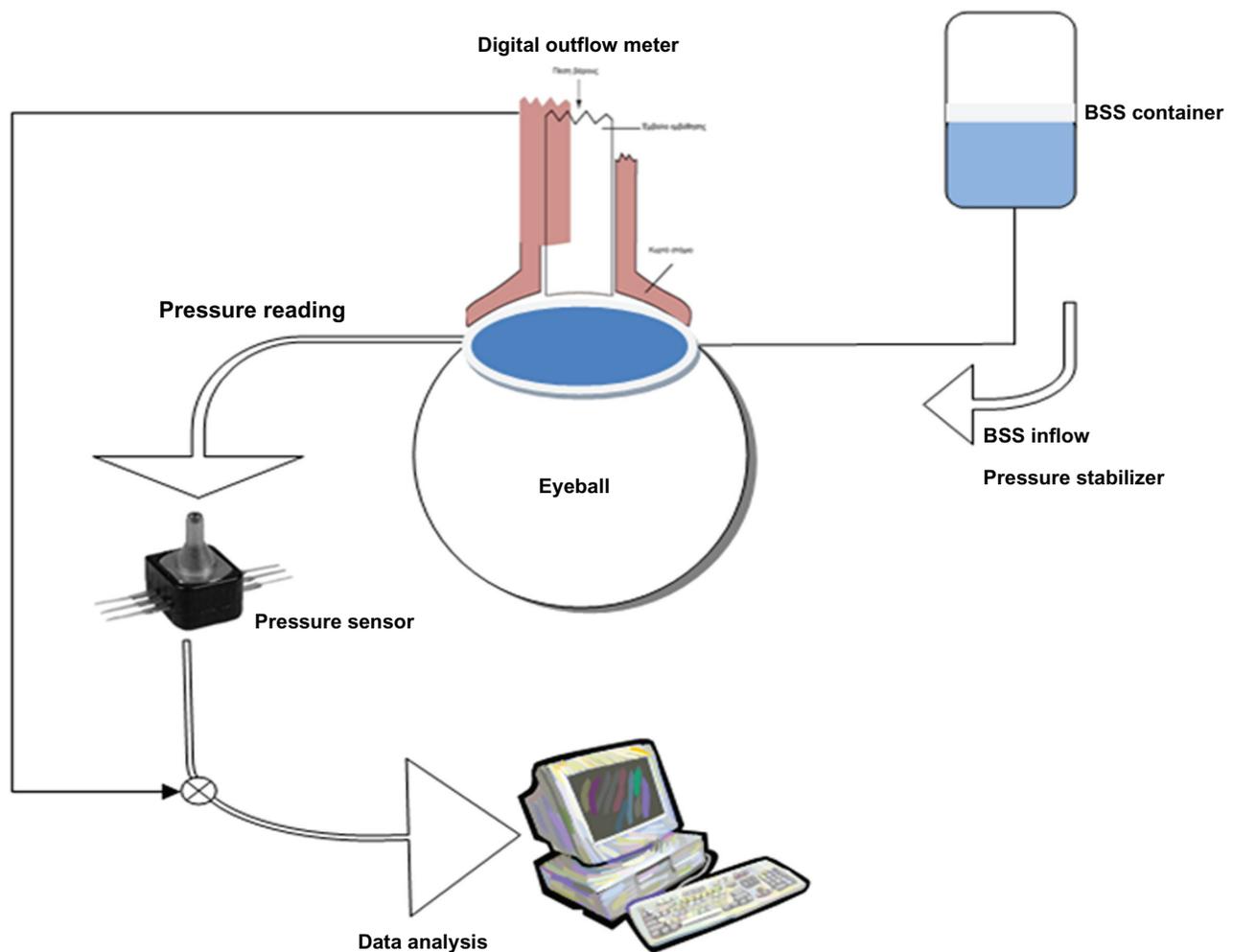
**Figure 4** Outflow facility windows software based on Java language. Outflow facility calculation software, designed in Java programming language with Windows® interface environment. Mandatory “inputs” are designed to measure the outflow facility, while “optional” inputs are designed to measure the ocular rigidity factor. “Corrected” outputs represent the outflow facility and rigidity measurements, corrected by the “optional” inputs. Correlation is a predictive algorithm of the severity of the condition from 0 to 3 for normal to acute angle closure, respectively.

where  $K_{age}$  is the rigidity variation based on the age of the patient;<sup>5</sup>  $K_{cct}$  is the rigidity variation based on central cornea thickness;<sup>4</sup>  $K_{refraction}$  is the rigidity variation based on the ocular axial length;<sup>4</sup> age is patient age in years; CCT is the central corneal thickness ( $\mu\text{m}$ ); and L is the ocular axial length (mm).

### Phase 3

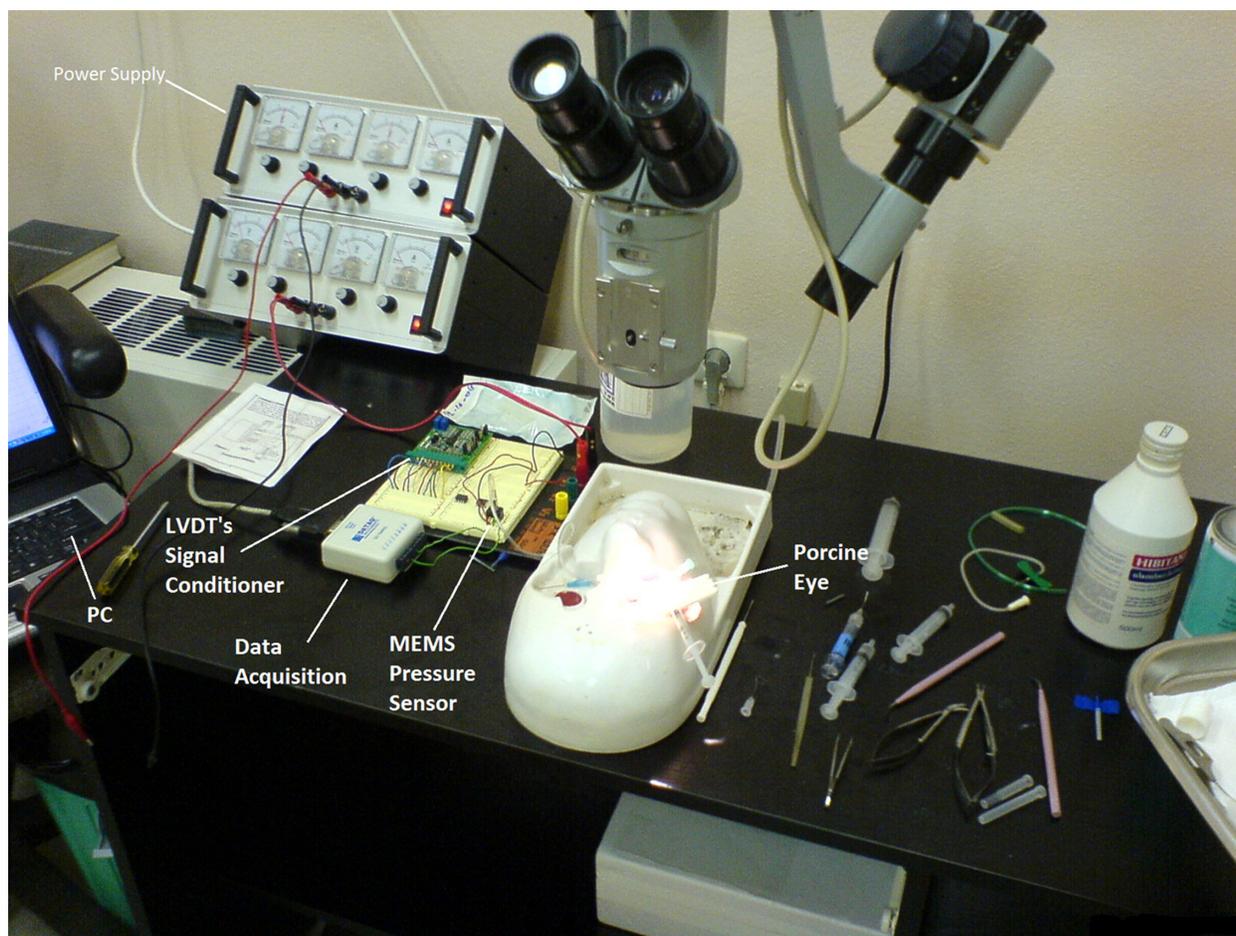
Phase 3 involved characterization and validation of the DAHOM. Characterization of the tonometer was accomplished using porcine cadaver eyes according to the following procedure. A microelectronic pressure sensor was implanted into the anterior chamber using a fine needle. A second needle was injected into the eye, connecting a water tank of balanced solution for IOP regulation, which was accomplished by altering the water tank height and thus affecting the hydrostatic pressure difference in the eye (Figures 5 and 6). Experimental IOP measurements were obtained in the range 5–90 mmHg, with a 1 mmHg increment.

Validation of the system was accomplished by comparing the measurement outcomes of the DAHOM with the corresponding ones of a Schiøtz tonographer in a population of 30 volunteers according to the following procedure. Outflow facility measurements were obtained in one eye using a Schiøtz tonographer and in the fellow eye by the DAHOM. Within one week, the procedure was repeated in a crossover manner. All tonography measurements were obtained by the same experienced operator (NF) who ensured proper eye fixation. Before each measurement, the Schiøtz tonographer was calibrated according to the manufacturer's instructions. GAT IOP measurements determined the indentation weight for both systems. For IOPs less than 30 mmHg, a 5.5 g weight was used, while a 7.5 g weight was used for IOP between 30 and 45 mmHg. For IOPs higher than 45 mmHg, a 10 g weight was used. The level of agreement between the two systems was evaluated by means of paired *t*-test and by Bland-Altman analysis. DAHOM repeatability was evaluated



**Figure 5** Laboratory setup for the characterization of the digital outflow meter.

Laboratory setup for the calibration of the system. The balanced solution (BSS) container is used for intraocular pressure regulation, the micropressure sensor is used for intracameral real-time intraocular pressure measurements, while the digital outflow meter performs tonography. All data are collected by the PC and analyzed.



**Figure 6** Experimental setup.  
Experimental setup in porcine cadaver eyes using a microelectromechanic intracameral pressure sensor.

by both Cronbach's alpha test and the intraclass correlation coefficient (ICC) from three consecutive measurements prior to the tonography study.

### Statistical analysis

Results were analyzed with the SPSS Version 17.0 (Statistical Package for the Social Sciences Inc., Chicago, IL). The normality of continuous variables was assessed using the Kolmogorov-Smirnov test. Quantitative variables expressed as mean  $\pm$  standard deviation (SD) and qualitative variables were expressed as frequencies and percentages. The Mann-Whitney test was used to assess outflow facility variations between the Schiottz and digital outflow meters. All tests were two-tailed, and statistical significance was considered as  $P < 0.05$ . Intrasession repeatability was tested using Cronbach's alpha test and the ICC. Agreement of the outflow facility measurements between the digital and Schiottz outflow meters was assessed with Bland-Altman plots and 95% limits of agreement. MedCalc version 9.0 software was used for the Bland-Altman plots.

### Results

The experimental setup with the porcine eyes provided the necessary data for the characterization of the system's response, according to the following formulae:

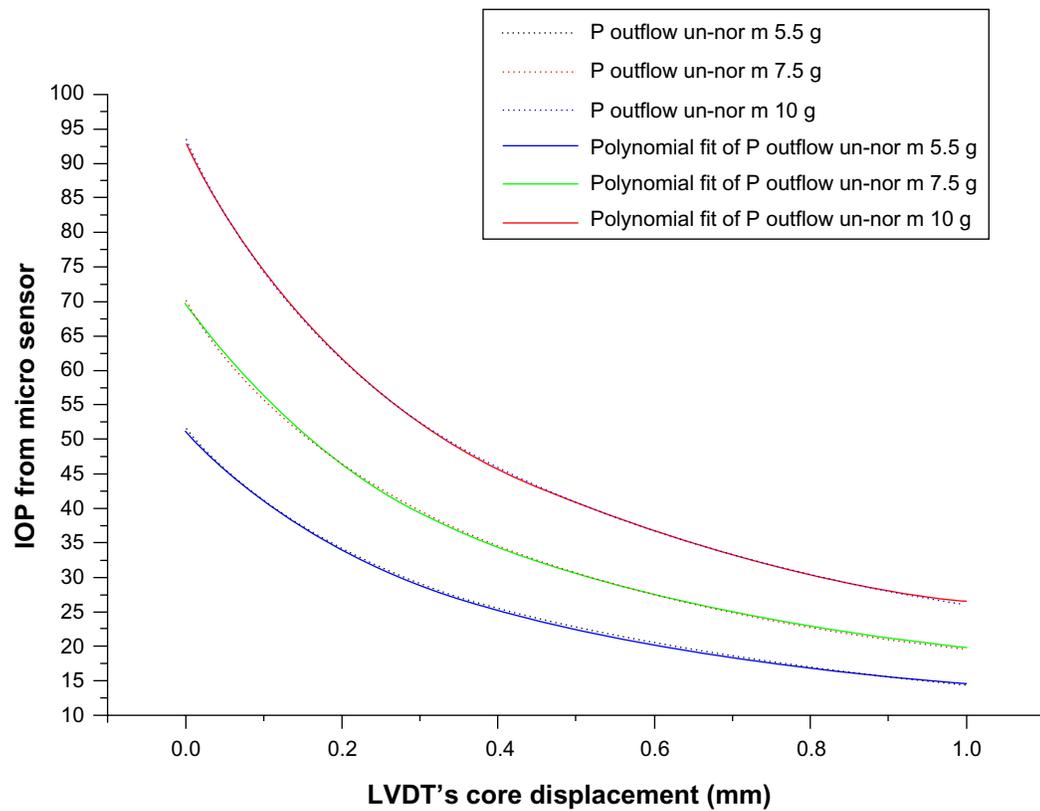
$$IOP_{MEMS} = 51.081 - 117.735x + 191.649x^2 - 171.753x^3 + 61.131x^4 \quad (F4)$$

$$IOP_{MEMS} = 69.668 - 160.908x + 262.05x^2 - 234.266x^3 + 83.266x^4 \quad (F5)$$

$$IOP_{MEMS} = 92.89 - 214.339x + 348.911x^2 - 312.038x^3 + 111x^4 \quad (F6)$$

where  $x$  is the magnitude of indentation for the DAHOM in mm.

In fact, the characterization of the DAHOM was accomplished using a fourth order polynomial equation (adjusted R-square  $>0.999$  in all polynomial fittings, Figure 7). Three different polynomial equations were derived, each one



**Figure 7** Indentation versus intraocular pressure intracameral readings from the microelectronic silicon-based pressure sensor. Objective intraocular pressure versus indentation measurements in an experimental setup using extracted porcine cadaver eyes. Intraocular pressure measurements attained by a micropressure sensor, connected to the anterior chamber of the eye, while the indentation measurements attained by the digital outflow meter.

corresponding to a different plunger weight. Systems transfer functions are shown below. Equation F7 was used for a 5.5 g plunger weight, F8 for 7.5 g, and F9 for 10 g:

$$y(x) = 51.081 - 117.735x + 191.649x^2 - 171.753x^3 + 61.131x^4 \quad (\text{F7})$$

$$y(x) = 69.668 - 160.908x + 262.05x^2 - 234.266x^3 + 83.266x^4 \quad (\text{F8})$$

$$y(x) = 92.89 - 214.339x + 348.911x^2 - 312.0.8x^3 + 111x^4 \quad (\text{F9})$$

It should be mentioned that all polynomials were derived by assessment of the best fitting of the experimental results in a Cartesian plot, with one axis representing the experimental measurements of interest and the second axis representing the values obtained by the DAHOM. The order of polynomial fitting was selected in a way to provide R-Square adjustment higher than 0.98, ensuring minimum calculation error.

DAHOM demonstrated a sufficient level of agreement with the Schiötz tonographer. Specifically, the results for DAHOM were:  $C_{\text{Digital}} \pm SD_{\text{Digital}} = 0.168 \pm 0.08 \mu\text{L} \times \text{min}^{-1} \times \text{mmHg}^{-1}$

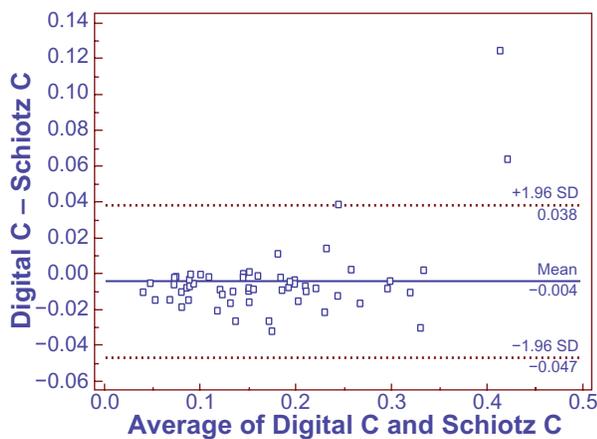
and for the Schiötz tonometer were:  $C_{\text{schiotz}} \pm SD_{\text{schiotz}} = 0.163 \pm 0.09 \mu\text{L} \times \text{min}^{-1} \times \text{mmHg}^{-1}$ ; Paired sample *t*-test validated measurements conformity ( $P > 0.12$ ). Sufficient level of agreement was also confirmed by Bland-Altman analysis. According to the plot in Figure 8, with the exception of two outlying values, the plot points are distributed in a symmetric manner about the “zero difference” line.

Regarding DAHOM’s measurement repeatability, the Cronbach’s alpha was 0.997 and the ICC was 0.987, both tests suggesting high intrasession reliability.

## Discussion

The objective of this study was to develop a digital aqueous humor tonographer that could provide valid information about the outflow facility and address a series of technical and design limitations of the conventional tonographers.

Various tonographers have been introduced during the past 60 years. First, Schiötz,<sup>7</sup> then Bock et al<sup>8</sup> and others<sup>9,10</sup> introduced tonographers for measuring the outflow coefficient, and in 1951, Gant reported the use of an electronic tonographer connected to a paper strip.<sup>11</sup>



**Figure 8** Bland-Altman plot showing interdevice difference plotted against mean measurements for each eye. Bland-Altman plot showing interdevice difference plotted against mean measurements for each eye. Dotted line, zero line. Blue solid line, mean difference and boundaries of the 95% limits of agreement.

Among the difficulties in the development of a reliable tonographer is its characterization. For characterization of the DAHOM, we developed an experimental setup introducing an intracameral pressure sensor in porcine cadaver eyes. Although cadaver porcine eyes have biomechanical properties similar to those of human eyes, a number of differences should be taken into consideration, ie, cadaver eyes may introduce measuring errors due to lack of blood volume displacement during the tonography study, and despite similar stress-strain patterns, human and porcine corneas demonstrate different stress relaxation properties.<sup>12</sup> However, neither of these differences interfered with the characterization or the validation process. In fact, both the Schiotz tonographer and DAHOM demonstrated very similar results in the majority of cases. The observed nonsignificant differences may well be attributable to the known Schiotz vulnerabilities regarding ocular rigidity assessment rather than to the design and/or implementation of the DAHOM project.<sup>13</sup> Specifically, the average indentation values obtained by both systems (Schiotz and DAHOM) did not reveal any significant differences. However, the outcomes of the DAHOM are corrected by a series of rigidity impact algorithms (which is not the case for the Schiotz tonographer). Regarding outflow facility, the DAHOM demonstrated similar results in a series of former studies that used different tonographers.<sup>14–20</sup>

Regarding DAHOM's intrasession variability, both Cronbach's alpha and ICC tests suggested excellent repeatability. Specifically, the ICC value of 0.987 is well above the minimal ICC value of 0.90 that the literature suggests to be adequate.<sup>21</sup> It is known that in tonography studies the intrasession variability is exacerbated mainly due to the loss of eye

alignment when retracting and placing the tonographer. In the software development of the DAHOM, we incorporated a software-based filter for automatic rejection of tracing irregularities that result in outlying values (Figure 3). However, hysteresis of the DAHOM was mainly attributed to the nonlinear semielastic properties of the eye, as shown in the report by Luce.<sup>22</sup>

Following the introduction of a reliable and valid tonographer like the DAHOM, its enhancements over the traditional tonographers should be underscored. The capability to provide raw data and outcomes measured in a digital format facilitates the processing and reprocessing of the data (both real-time and at a later time), allows introduction of different filters for cutting off measurement irregularities, and facilitates tonographic follow-up of patients because point-to-point comparisons can be made over time. The capability to calculate ocular rigidity and incorporate its impact on every single measurement on final measured outcome is a major advance over traditional designs that assume a mean ocular rigidity value for their calculations. Moreover, there is the capability to correct the measured outcome of the DAHOM by estimation of the impact of a series of optional ocular biomechanical factors and patient age.

In summary, in this report we present a characterization and validation of the DAHOM, a novel digital aqueous humor tonographer that attempts to address the known inherent vulnerabilities of the traditional tonographers. Addressing these vulnerabilities will allow the implementation of future relevant studies with high clinical significance in diseases with disrupted aqueous humor outflow, eg, the glaucomas. Among them are the qualitative outflow profile analysis that could provide detail information of the dynamic regulation of the outflow facility,<sup>23–26</sup> and the development of a glaucoma risk assessment algorithm, capable of identifying preclinical patterns of glaucoma development.

## Disclosure

The authors report no conflict of interest in this work.

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