

# Nomogram Based on Ultrasonography and Clinical Features for Predicting Malignancy in Soft Tissue Tumors

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**Purpose:** The objective of this study was to establish a predictive nomogram based on ultrasound (US) and clinical features for patients with soft tissue tumors (STTs).

**Patients and Methods:** A total of 260 patients with STTs were enrolled in this retrospective study and were divided into a training cohort (n=200, including 110 malignant and 90 benign masses) and a validation cohort (n=60, including 30 malignant and 30 benign masses). Multivariate analysis was performed by binary logistic regression analysis to determine the significant factors predictive of malignancy. A simple nomogram was established based on these independent risk factors including US and clinical features. The predictive accuracy and discriminative ability of the nomogram were measured by the calibration curve and the concordance index (C-index).

**Results:** The nomogram, comprising US features (maximum diameter, margin and vascular density) and clinical features (sex, age, and duration of disease), showed a favorable performance for predicting malignancy, with a sensitivity of 88.2% and a specificity of 78.7%. The calibration curve for malignancy probability in the training cohort showed good agreement between the nomogram predictions and actual observations. The C-indexes of the training cohort and validation cohort for predicting malignancy were 0.89 (95% CI: 0.85–0.94) and 0.83 (95% CI: 0.73–0.94), respectively.

**Conclusion:** The nomogram based on US and clinical features could be a simple, intuitive and reliable tool to individually predict malignancy in patients with STTs.

**Keywords:** soft tissue tumors, ultrasonography, malignancy, predictive model, nomogram

## Introduction

Soft tissue tumors (STTs) are fairly common and heterogeneous clinical entities.<sup>1</sup> Their pathologic classification and nomenclature are complicated. The ratio of malignant to benign STTs has been estimated to be nearly 1:100.<sup>2</sup> Some malignant STTs are often misdiagnosed as benign STTs owing to many overlaps in clinical and imaging manifestations among them, resulting in inadequate management, such as unplanned resections.<sup>3</sup> To make a definite diagnosis of STTs, biopsy should be performed in suspected cases. However, routine biopsy for each entity is not practical. Thus, an optimal process for the diagnosis and management of STTs is regarded as a clinically challenging problem that needs to be addressed.

US is an imaging modality with availability, portability and low cost that has become an important complementary tool for musculoskeletal imaging.<sup>4</sup> Patients with soft tissue masses are referred for US to confirm the exact layer, identify the boundary

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and margin, measure the size, estimate the vascularity and determine the relationship between the masses and surrounding tissues. With the rapid development of sonography technology, the resolution of grayscale US and the capability of color Doppler flow imaging (CDFI) to depict vascular anomalies have been greatly improved. Thus, US can provide more useful information for discerning malignant lesions from benign lesions and even for the pathological diagnoses of STTs, and it has become the first-line examination in clinical practice.<sup>5,6</sup> To date, there have been many studies with relatively small samples addressing the accuracy of US in distinguishing benign and malignant STTs. In earlier studies, the accuracy of US for recognizing malignancy in STTs ranged from 69% to 93% by employing many US parameters, such as size, tumor margin, fascia layer, and vascular pattern.<sup>7-9</sup>

However, among the many meaningful US parameters for identifying malignancy, there is statistical inconformity in the value of each parameter. Thus, there is a great need for the development of predictive models for the differential diagnosis of benign and malignant STTs by statistically weighting the contributions of the many US parameters. And what is more, there is no unified standard or model in differentiating benign and malignant STTs similar to Thyroid Imaging Reporting And Data System (TI-RADS) or Breast Imaging Reporting And Data System (BI-RADS) which is the only point of reference in thyroid or breast imaging system.

A nomogram can give rise to a numerical probability of a clinical event, such as malignant tumor, by creating an intuitive graph of a statistical predictive model.<sup>10</sup> It has been accepted as a reliable tool to quantify risk by incorporating and illustrating important factors for malignancy.<sup>10-12</sup> So far, nomograms have been established in the majority of cancer types.<sup>10-13</sup> For instance, Guo et al developed an US-based nomogram to improve the diagnostic accuracy of the identification of malignant thyroid nodules;<sup>14</sup> Qiu et al established and validated a nomogram to predict the probability of axillary lymph node metastasis as a preoperative tool to support clinical decision-making.<sup>15</sup> To the best of our knowledge, this study is the first attempt to develop and validate a nomogram based on US parameters as well as clinical risk factors to predict malignant STTs.

## Patients and Methods

### Patients and Data Acquisition

This retrospective study was carried out according to the ethical standards of the Declaration of Helsinki and was

approved by the ethics committee of the First Affiliated Hospital of Nanjing Medical University. The requirement for obtaining informed consent from individual participants was waived, and the participants' privacy and personally identifiable information were protected. From January 2018 to April 2020, a total of 429 patients with STTs who underwent both US examination and core biopsy (or open surgical biopsy) were retrospectively reviewed. All the cases came from the interventional US clinic where radiologists performed US/CEUS guided interventional procedures.

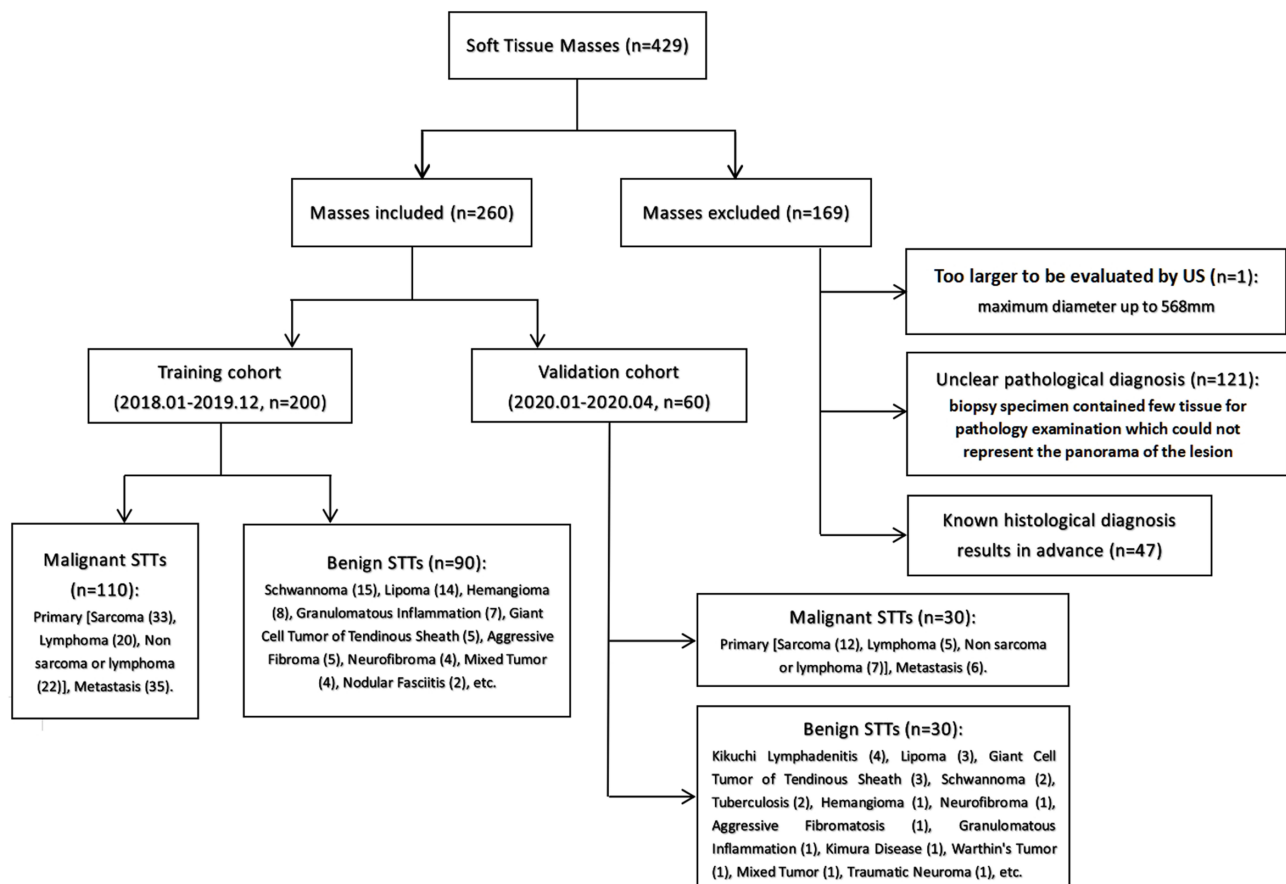
Among the 429 patients examined, 169 were excluded because the mass was too large to be evaluated by US (n=1), the histological diagnosis was known in advance (n=47) or the pathological diagnosis was unclear (n=121) in this study. Ultimately, 260 pathologically confirmed STTs were grouped into the training cohort (n=200) and validation cohort (n=60) according to the order of the examination time. A total of 200 patients, including 110 malignant and 90 benign masses diagnosed between January 1, 2018, and December 31, 2019, were included as the training cohort, and 60 patients, including 30 malignant and 30 benign masses diagnosed between January 1, 2020, and April 30, 2020, were included as the validation cohort (Figure 1). The clinical characteristics of the patients, including age, sex, duration of disease and histologic type of tumor, were obtained from the medical records.

The malignant rate and median age of the training cohort vs validation cohort were 55.0% vs 50.0% and 55.0 years (range, 15–88 years) vs 55.5 years (range, 14–78 years), respectively, which were not significantly different. The male-to-female ratio of the training cohort and validation cohort was 1.2:1 and 1.1:1, respectively.

### US Examination

All US examinations were performed by two experienced musculoskeletal radiologists. A LOGIQ E9 (GE Healthcare, Milwaukee, WI, USA) ultrasound instrument with a C1-6VN convex transducer (2–6 MHz) and ML linear transducer (6–15 MHz) was used. The ultrasound gel and light pressure on the probe for the lesion area were needed to avoid excessive compression of the mass and optimize the color flow display.

All grayscale and color Doppler flow images were reviewed by two radiologists who had 5 and 10 years of experience in musculoskeletal ultrasound. To minimize selection bias regarding diagnostic accuracy, they needed to reach an agreement on the US reports. The following



**Figure 1** Flow diagram of the study participants.

characteristics were evaluated and recorded: (1) echogenicity (relative to muscle: predominantly hypoechoic, predominantly isoechoic, or predominantly hyperechoic); (2) internal content (predominantly solid (cystic portion  $\leq 10\%$  of the mass volume), mixed (cystic portion  $>10\%$  but  $\leq 50\%$ ), or predominantly cystic (cystic portion  $>50\%$ )); (3) echotexture (homogeneous or heterogeneous); (4) shape (regular, lobulated, or irregular); (5) boundary (well defined: clear-cut and thin capsule-like; undefined: uncertain margin with respect to adjacent normal tissue; partially defined: case between the both above); (6) margin (smooth: characterized by an even, gradually curving interface; spiculate: lobulation, angulation, or intrusion of the lesion's solid component into the surrounding tissue is present to any extent; rough: characterized by irregular and rough curving interface); (7) location (head or neck, trunk, upper limb, or lower limb); (8) layer (superficial fascia layer or deep fascia layer); (9) calcification (absent; microcalcifications:  $<0.5$  mm; macrocalcifications:  $\geq 0.5$  mm); (10) vascular density (grade 0, I, II, or III); (11) vascular type (absent, predominantly central, predominantly peripheral, or mixed); and (12) maximum diameter. Spectral

wave analysis and elastography were not routinely performed.

The lesion depth was characterized as superficial or deep relative to the investing fascia as identified on US. Superficial soft tissue masses are those that are located superficial to the investing fascia.<sup>16</sup>

Settings for CDFI are as follows: the scale level and pulse repetition frequency were decreased, the color gain was increased until color noise became apparent; radiologists adjusted the value of color gain and speed scale according to the blood flow velocity in each lesion, in order to achieve the best visual effect without overflow or interruption of blood flow signal. The pressure of the transducer on the lesion was lowered to avoid compressing the small vessels, which may cause low velocity signals to disappear.

The vascular density on CDFI was graded according to the semiquantitative method of Adler et al as follows:<sup>17</sup> (1) grade 0, no obvious blood flow in the mass; (2) grade I, only minimal blood flow, such as 1 to 2 punctate or rod-shaped blood flows in the mass; (3) grade II, moderate vascularity, such as 3 to 4 punctate blood flows or an

important blood vessel that can be detected in the mass; and (4) grade III, marked vascularity, such as more than 4 blood vessels or vessels interwoven into a network.

## Biopsy

A 16-G needle was used in the US/CEUS-guided biopsy. After identifying the needle tip was in the mass, operator pulled the trigger, took 3–4 pieces of tissue and sent them to the department of pathology for examination.

## Pathology Examination

The samples were submitted to the department of pathology. After being fixed in formalin, embedded in paraffin, and stained with HE, these specimens were taken for routine histopathological examination and some of them even for immunohistochemistry. All specimens were reviewed according to ESMO guidelines<sup>18</sup> by two pathologists who were experts in sarcoma in order to confirm the diagnosis. Each case with uncertain biopsy results would be recommended for surgery.

## Statistical Analysis

Descriptive statistics are shown as the median and range for continuous variables and as the number of participants for categorical variables. Continuous variables of age, duration of disease and maximum diameter of STTs were transformed into categorical variables based on cutoff values before modeling. The cutoff values were evaluated using receiver operating characteristic (ROC) analyses. Categorical variables were compared using the chi-square test. Variables that achieved significance in the univariate analysis were entered into the multivariable analysis via the binary logistic regression model.

Statistical analyses to identify independent risk factors for malignancy were performed by SPSS software, version 23.0 (IBM Corporation, Armonk, NY). A *P* value <0.05 was considered statistically significant.

## Construction of the Nomogram

In accordance with the results of the multivariable analysis, a simple nomogram of clinical and US characteristics was established by R software (Windows version 3.6.1) with the rms package.

## Calibration and Validation of the Nomogram

Calibration of the nomogram for predicting malignancy was performed by comparing the predicted probability

with the observed probability after bias correction. The model performance for predicting malignancy was assessed by calculating the concordance index (C-index).<sup>19</sup> The larger the C-index, the more accurate was the prediction.<sup>20</sup> The value of the C-index ranges from 0.5 to 1.0, with 0.5 representing a random chance and 1.0 representing a perfect ability to correctly differentiate the outcome with the model.

Afterward, a validation cohort was used for external validation. Bootstraps with 1000 resample were used for these activities.

## Results

### Clinical and US Characteristics of the Patients

Overall, the distributions of the following variables in the validation cohort were basically the same as those in the training cohort, with slight differences among the 15 features: sex, age, duration of disease, maximum diameter, location, fascia layer, shape, boundary, margin, echogenicity, echotexture, internal content, calcification, vascular density and type. The details of the respective numbers with US and the clinical features of the training and validation cohorts are listed in [Tables 1](#) and [2](#).

The cutoff values for age, maximum diameter and duration of disease were 62.5 years, 58.5 mm and 11 months, respectively.

### Diagnostic Efficacy of Clinical Features Combined with US Parameters vs US Parameters Alone

Binary logistic regression analysis was performed for predicting malignancy in STTs based on clinical features combined with US parameters and based on US parameters alone. The forest plot showed that sex (OR=0.387, *p*=0.024), age (OR=4.607, *p*=0.002), duration of disease (OR=0.293, *p*=0.012), maximum diameter (OR=3.430, *p*=0.006), margin (OR=3.364, *p*=0.012), and vascular density (OR=2.849, *p*=0.000) were independent risk factors of malignancy prediction in STTs in the former study ([Figure 2A](#)); we re-evaluated all cases using the US parameters alone, which indicated that maximum diameter (OR=3.010, *p*=0.007), margin (OR=4.090, *p*=0.001), and vascular density (OR=2.879, *p*=0.000) were independent risk factors of malignancy prediction in STTs ([Figure 2B](#)).

The ROC curves of the clinical features combined with US parameters predictive model and US parameters

**Table 1** Clinical Features of Patients with STTs

Clinical Characteristics	Training Cohort (n=200)		Validation Cohort (n=60)	
	No. of Patients	%	No. of Patients	%
Pathological Classification				
Malignant	110	55.0	30	50.0
Benign	90	45.0	30	50.0
Sex				
Male	90	45.0	31	51.7
Female	110	55.0	29	48.3
Age (years)				
Median	55.0		55.5	
Range	15–88		14–78	
Duration of Disease (months)				
Median	3.0		2.0	
Range	0.2–240.0		0.2–48.0	
Maximum Diameter (mm)				
Median	46.0		33.5	
Range	9–213		13–200	
Location				
Head or Neck	48	24.0	22	36.7
Trunk	71	35.5	15	25.0
Upper Limb	20	10.0	0	0.0
Lower Limb	61	30.5	23	38.3

alone predictive model in the training cohort were plotted as shown in [Figure 3](#), and the AUC was 0.896 (95% CI: 0.851–0.941) and 0.851 (95% CI: 0.798–0.903), respectively. This result suggested that the predictive model which clinical features combined with US parameters was more accurate and useful for determining the malignancy of STTs.

## Establishment of the Nomogram for Malignancy

With the logistic regression analysis of the predictive model which clinical features combined with US parameters, the independent risk factors for malignant STTs were integrated into a nomogram. With this nomogram, a patient is assigned a score on the points axis for each variable. After adding the total score, the numerical value on the total points axis can be located. Then, we can draw a straight line downward to the risk axis to determine the estimated probability of malignancy ([Figure 4](#)).

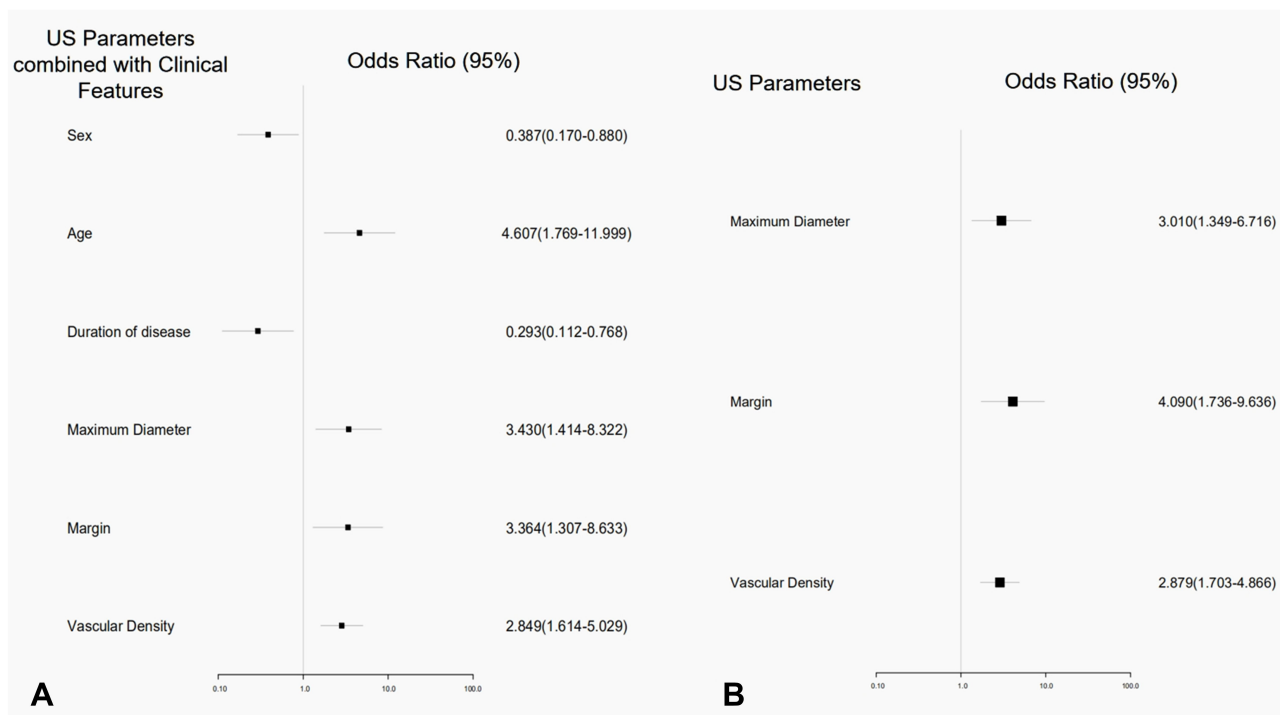
**Table 2** US Features of Patients with STTs

US Characteristics	Training Cohort (n=200)		Validation Cohort (n=60)	
	No. of Patients	%	No. of Patients	%
Echogenicity				
Pred. Hypoechoic	180	90.0	54	90.0
Pred. Isoechoic	5	2.5	1	1.7
Pred. Hyperechoic	15	7.5	5	8.3
Internal Content				
Pred. Solid	178	89.0	55	91.7
Pred. Cystic	3	1.5	1	1.6
Mixed	19	9.5	4	6.7
Echotexture				
Homogeneous	29	14.5	20	33.3
Heterogeneous	171	85.5	40	66.7
Shape				
Regular	45	22.5	34	56.7
Lobulated	95	47.5	15	25.0
Irregular	60	30.0	11	18.3
Boundary				
Well defined	96	48.0	37	61.7
Partially defined	90	45.0	18	30.0
Undefined	14	7.0	5	8.3
Margin				
Smooth	58	29.0	31	51.7
Spiculate	104	52.0	20	33.3
Rough	38	19.0	9	15.0
Fascia Layer				
Superficial	40	20.0	21	35.0
Deep	160	80.0	39	65.0
Calcification				
Absent	160	80.0	56	93.3
Micro	7	3.5	4	6.7
Macro	34	17.0	0	0.0
Vascular Density				
Grade 0	32	16.0	11	18.3
Grade I	68	34.0	19	31.7
Grade II	66	33.0	23	38.3
Grade III	34	17.0	7	11.7
Vascular Type				
Absent	32	16.0	4	6.6
Pred. Central	34	17.0	28	46.7
Pred. Peripheral	78	39.0	16	26.7
Mixed	56	28.0	12	20.0

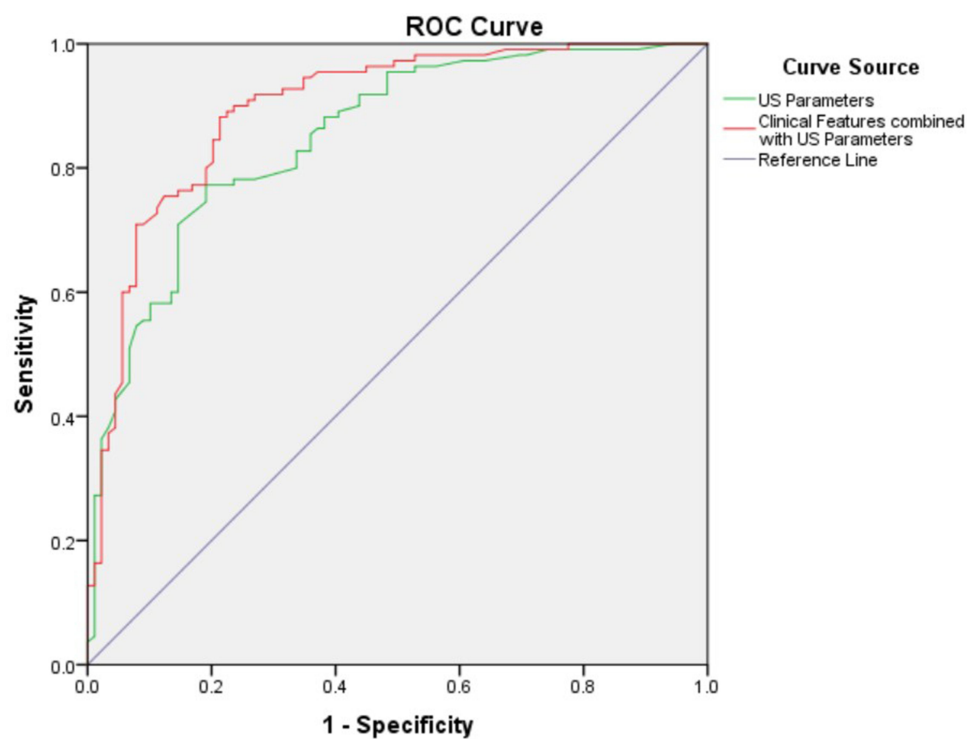
**Abbreviation:** Pred, predominantly.

## Calibration and Validation of the Nomogram

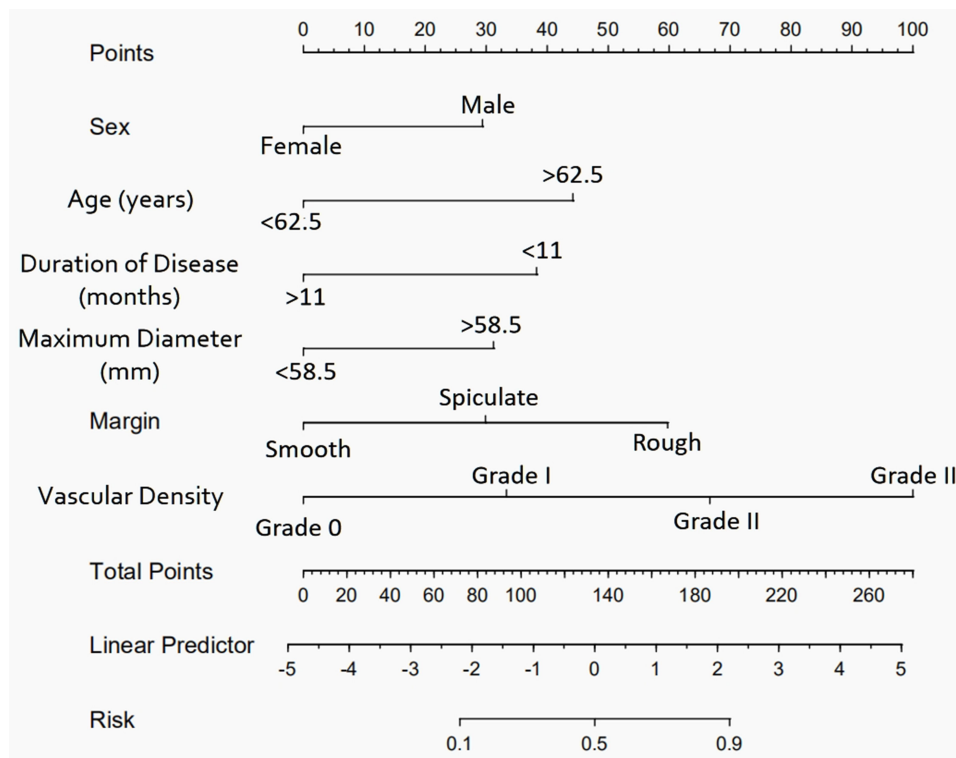
The calibration curves displayed excellent agreement between the prediction and actual observation in the



**Figure 2** Independent risk factors for malignancy of predictive models in forest plots of multivariate analyses. **(A)** US parameters combined with clinical features predictive model. **(B)** US parameters alone predictive model.



**Figure 3** The ROC curves of the clinical features combined with US parameters predictive model (red line) and US parameters alone predictive model (green line). The AUC was 0.896 (95% CI: 0.851–0.941) and 0.851 (95% CI: 0.798–0.903), respectively.



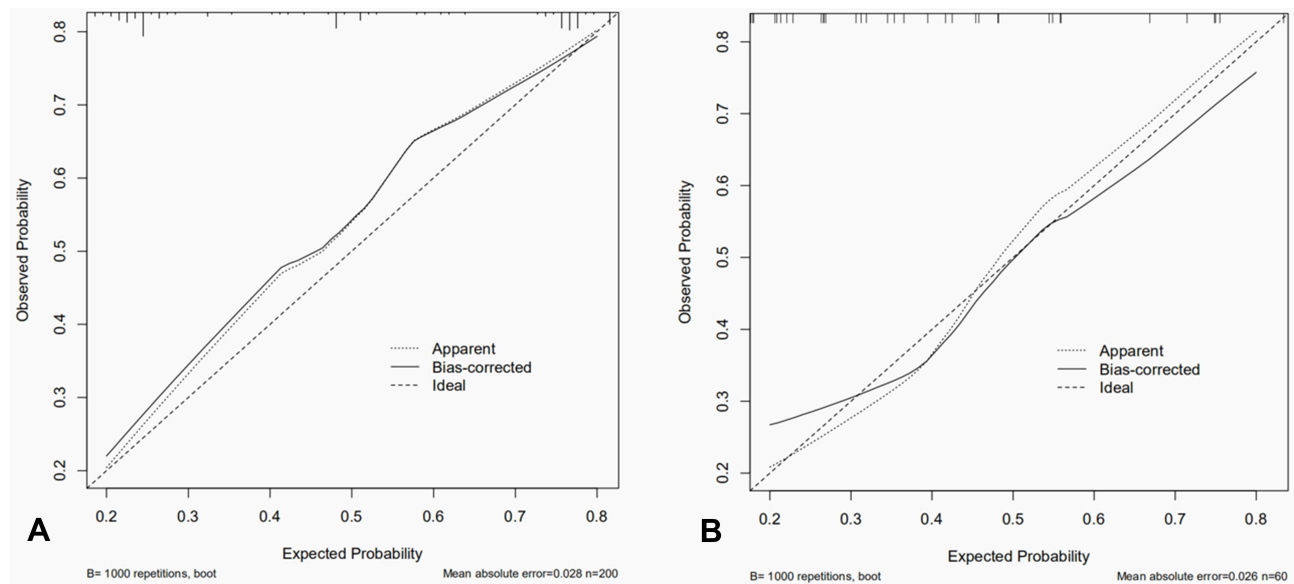
**Figure 4** The nomogram of the predictive model for malignancy in patients with STTs. To use this nomogram, an individual patient's value is located on each variable axis, and a line is drawn upward to determine the number of points received for each variable value. The sum of these numbers is located on the total points axis, and a line is drawn downward to the Risk axis to determine the likelihood of malignancy.

training cohort (Figure 5A) and acceptable agreement in the validation cohort (Figure 5B).

The C-index of the established nomogram for malignancy prediction was 0.89 (95% CI: 0.85–0.94) in the

training cohort and 0.83 (95% CI: 0.73–0.94) in the validation cohort.

Typical Examples of US Presentations of Benign and Malignant STTs (see Figures S1 and S2).



**Figure 5** The calibration curve of the nomogram for predicting malignancy. (A) Training cohort. (B) Validation cohort. The nomogram prediction of malignancy is plotted on the X-axis, and the actual observation is plotted on the Y-axis. Solid and dotted lines in calibration curves correspond to calibrating-predictive (bias-corrected) and predictive (apparent) values. Dashed lines correspond to standard (ideal) values.

## Discussion

The pathological classification of STTs is complex, and the imaging manifestations vary, which makes qualitative diagnosis especially difficult. Many physicians consider core biopsy to be a simple, low-risk procedure with a diagnostic accuracy ranging from 80.7% to 96.9% for STTs.<sup>21,22</sup> Some specialists even suggest that biopsy should be performed promptly in patients with a high risk of malignancy.<sup>23,24</sup> However, conducting biopsy examination in each patient is not practical, and it may induce some complications. Thus, how to screen high-risk patients for biopsy with a simple method is still a serious problem that needs to be solved.

US has a good resolution with soft tissues and can provide information on lesion size, location and depth, as well as the relationship of the lesion with surrounding tissues. In recent years, with the wide application of US in STTs and prolific experience accumulated by doctors, the diagnostic accuracy of US in the assessment of STTs has been significantly improved.<sup>8,25</sup> To the best of our knowledge, despite several formerly reported predictive models for malignant STTs according to US findings, no nomogram based on US features has been established. Thus, in this work, we developed a simple and intuitive nomogram integrating US and clinical characteristics to predict the malignant rate of patients with STTs. This predictive model contained more cases and fewer variables, so it is reliable, easy to carry out and generalizable and has a relatively high accuracy. We expect the nomogram to be able to make individualized predictions of the malignant rate, screen out more patients with malignancy, reduce unnecessary biopsies and help patients and surgeons make better decisions in the clinical diagnosis and treatment process.

The training cohort and validation cohort were obtained from the interventional US clinic. These patients who came here for consultation were generally the cases that had been discussed beforehand in orthopaedic clinic or general surgery clinic by the surgeons but had no preliminary diagnosis, which represented the complexity of the cases. If the possibility of malignancy could not be completely ruled out either by two or more radiologists with more than five years of working experience in our interventional US clinic, then the patients should be recommended to perform biopsy or surgery and they were always well prepared in the mind to undergo them.

Figure 3 indicates that the predictive model in which clinical features combined with US parameters is more useful for determining the malignancy of STTs, and the diagnostic efficacy has improved by combining clinical factors. So we established a nomogram using the clinical features combined with US parameters in this study.

The nomogram showed that the independent risk factors for malignant STTs included vascular density, margin, maximum diameter, duration of disease, age and sex. The vast majority of these findings were generally similar to those of previous studies,<sup>7,25,26</sup> which reported risk factors including rough margin, maximum diameter, deep fascial layer, heterogeneous echotexture, and abundant vascularization.

Notably, from this nomogram, we could see that Grade III vascular density made the largest contribution to the malignancy prediction, followed by rough margin. Nagano et al<sup>27</sup> found that when type III (hypervascular with multiple peripheral poles) and type IV (hypervascular with internal vessels) vascularity of Giovagnorio's criteria<sup>28</sup> were taken as markers of malignancy, the specificity reached up to 91.0%. Morii et al<sup>25</sup> also reported that type III/IV vascularity (Giovagnorio's criteria) was associated with a high risk of malignant STTs. In our study, grade II/III vascular density with the Adler criteria was significantly associated with malignancy. Nagano and Morii classified the intratumoural blood flow according to Giovagnorio's criteria, while in our study, the Adler criteria were applied. The former criteria include vascular density and vascular type, while the latter only includes vascular density. In terms of vascular density, type III/IV of Giovagnorio's criteria are the same as grade II/III of the Adler criteria.

For the margin of the tumor, we agreed with Morii et al<sup>25</sup> and Oebisu et al<sup>7</sup> who suggested that an ill-defined margin of STT was considered malignant.

In this nomogram, malignant STTs showed obvious male predominance, which was consistent with the findings of De Marchi et al.<sup>26</sup> Largest diameter of the tumor  $\geq 50$  mm is a universally used parameter for malignant STTs.<sup>7,18,29</sup> Our results also supported this view and obtained a cutoff point of 58.5 mm.

The parameter of deep fascia layer has been frequently mentioned for predicting malignancy in STTs.<sup>29–31</sup> Previous studies such as those of Datir et al<sup>32</sup> and Alexander et al<sup>33</sup> showed that the percentage of malignant STTs in the superficial fascia layer was only 19.0% and 3.7%, respectively. However, the layer was not



incorporated into this nomogram. De Marchi et al also found that malignant STTs had no correlation with deep fascia layer.<sup>29</sup> To determine the reason, we analyzed the final pathological results of benign STTs (Figure 1) and found that in the top five common diseases (ie, schwannoma, lipoma, hemangioma, granulomatous inflammation, and giant cell tumor of tendon sheath), 75.5% (37/49) were located in the deep fascia layer. Therefore, it seemed to be related to the background of sample selection.

Nomogram validation is essential to avoid overfitting of the model and determine its generalizability.<sup>34</sup> The calibration curves of this study show that the nomogram prediction is consistent with the actual observation for malignant STTs, which indicates the repeatability and reliability of the established nomogram. The discrimination was revealed and the prediction was supported by the significantly high C-index of the established nomogram in the training cohort (0.89, 95% CI: 0.85–0.94); in the external validation cohort, the discriminative ability was slightly reduced with the C-index of 0.83 (95% CI: 0.73–0.94). We speculate that the sample size could be the main contributor to this difference; another reason might be that some different pathological types of STTs were included in the validation cohort, whereas such types were not included in the training cohort.

Nevertheless, there are several limitations in this study. First, the heterogeneity of STTs is the main reason, and various patients with benign lesions may be missed because they might not like to undergo core biopsy or open surgical biopsy. Second, the nomogram does not incorporate other US variables, such as blood flow velocity, resistance index, elastography, CEUS, and so on. Last, the US reporting criteria of this study only represent the local level, and the nomogram has not been tested in samples from other regions, so its authenticity and true effectiveness need more verification. Further efforts on multicenter, prospective data collection and patient follow-up, wider geographic recruitment, and the incorporation of more clinical and US factors are needed in the future.

## Conclusion

US features (maximum diameter, margin and vascular density) and clinical features (sex, age, duration of disease) were independent risk factors for malignant STTs. This nomogram based on these US and clinical characteristics has good accuracy in predicting the malignant rate of individual patients with STT, and it is worthy of being developed and generalized.

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## Disclosure

The authors report no conflicts of interest in this work.

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